

SPECT imaging of ^{161}Tb and ^{155}Tb and impact of ^{156}Tb pollution on image quality

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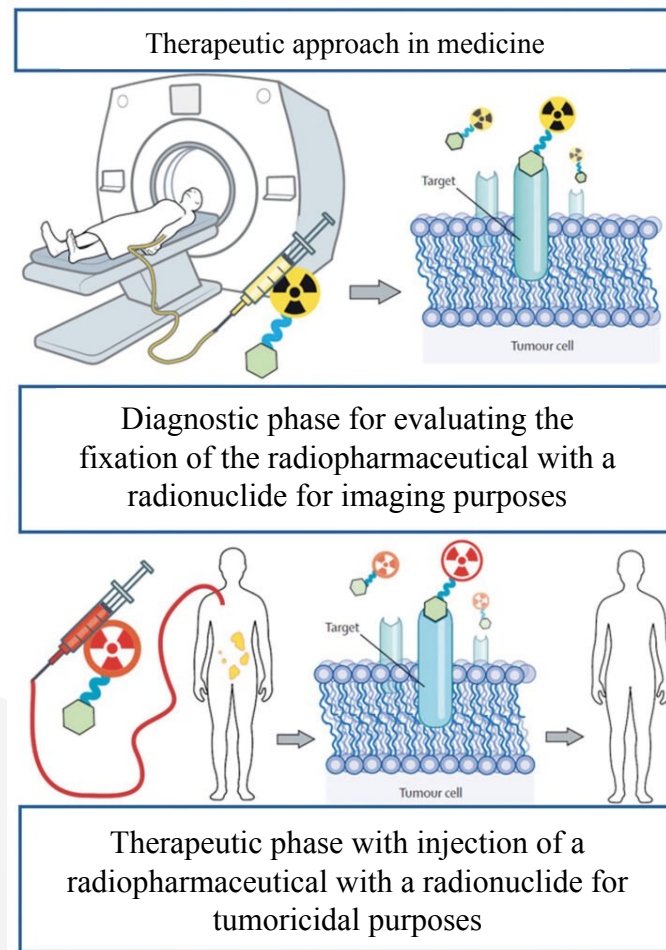
d: Institute of Radiation Physics, University Hospital of Lausanne, Lausanne, Switzerland.

- Vectorized internal radiotherapy (VIR) involves injecting radionuclide isotopes to target and treat cancer.
- To develop new VIR radiotracers, particularly those enabling a **theranostic** (therapeutic + diagnostic) approach.
- Terbium (Tb) features four key isotopes ideal for theranostic applications in nuclear medicine¹.

Isotope	Diagnosis	Therapy	1/2 life
¹⁴⁹ Tb	? β ⁺ 14.2% , γ	α	4.118 h
¹⁵² Tb	β ⁺ (PET)		17.5 h
¹⁵⁵ Tb	γ (SPECT)		5.32 d
¹⁶¹ Tb	Low energy γ (47.5 keV, 74.6 keV)	β ⁻	6.89 d

Potential
theranostic pair

Potential
theranostic pair



¹ Naskar N, Lahiri S. Theranostic Terbium Radioisotopes: Challenges in Production for Clinical Application. Front Med (Lausanne). 2021 May 31;8:675014.

- **PRALINE** project: **P**roduction **RA**dioisotopes et **L**igants pour l'**I**magerie **NucléairE**

- Aims to develop new methodologies of radioisotopes production, and develop approaches and methods for nuclear imaging (and new ligands).

- PRALINE-Imaging (SPECT) sub-project **Objectives**:

- Study ^{161}Tb SPECT imaging capability.
- Evaluate the impact of ^{156}Tb contamination (co-produced with ^{155}Tb) on quantitative ^{155}Tb SPECT imaging (same $T_{1/2}$), and acceptable contamination limit in ROI [60, 125] keV.

- **Methodology**:

- SPECT imaging experiment of ^{161}Tb .
- SPECT imaging exp. of: pure (^{155}Tb) and contaminated ($^{155}\text{Tb} + ^{156}\text{Tb}$).
- Monte Carlo simulation validated by the experiments.

Gamma rays (keV)		
^{161}Tb	^{155}Tb	^{156}Tb
25.65(23.2%)	86.54 (32%)	88 (18%)
48.92 (17.0%)	105.3 (25.1%)	199.2 (41%)
74.56 (10.2)	180.1 (7.5%)	356.3 (13.6%)
	262.3 (5.3%)	534.3 (67%)
		1065.1 (10.8%)
		1154.1 (10.4%)
		1222.4 (31%)
		1421.7 (12%)

- Detector: ALBIRA S108 small animal PET/SPECT/CT
(industrial) imaging system (BRUKER)¹.

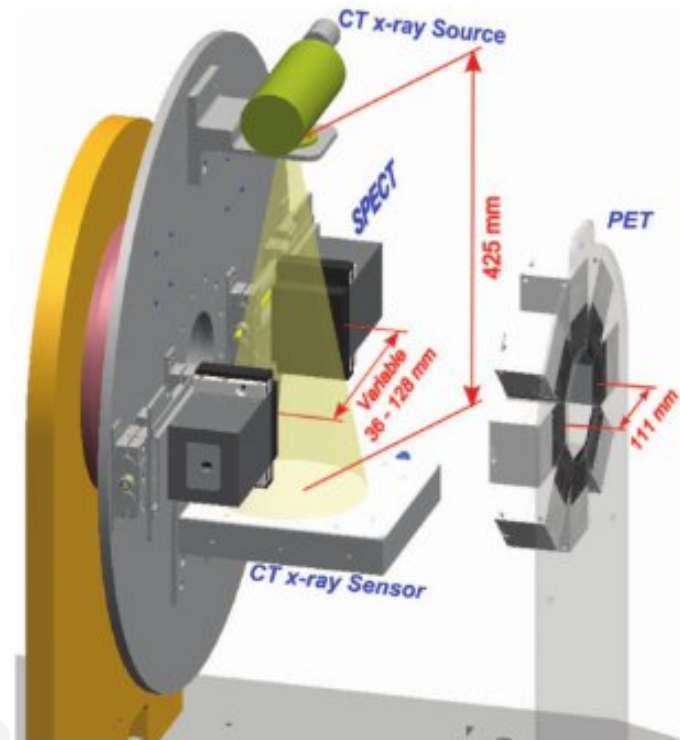
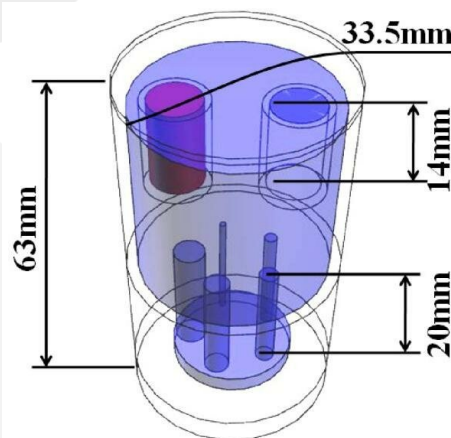
- 2 rotating SPECT heads, 30 positions/camera (6°).

- Camera optimized for ^{99m}Tc (140 keV).
- Single pinhole collimator (2 mm W).
- Spatial Res.(FWHM) : ~ 1.5 mm (BRUKER).

- Tomo-Reconstruction program implemented.

- Phantom: NEMA NU 4-2008 phantom².

- **Study and understand camera performance, include corrections in reconstruction.**

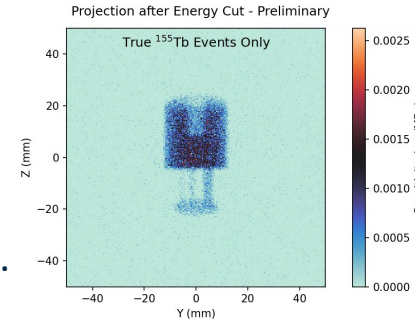


¹ Sánchez et al. Med. Phys, 40, No. 5, May 2013.

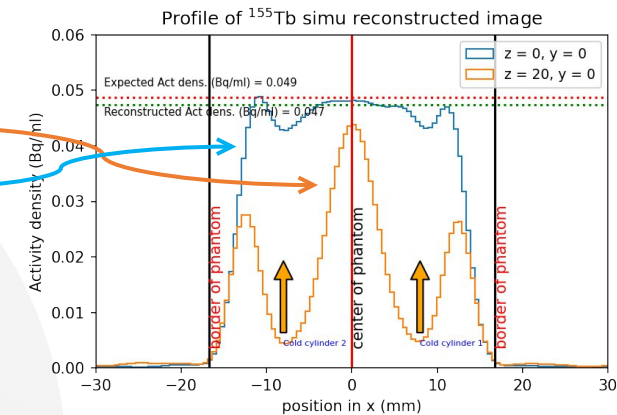
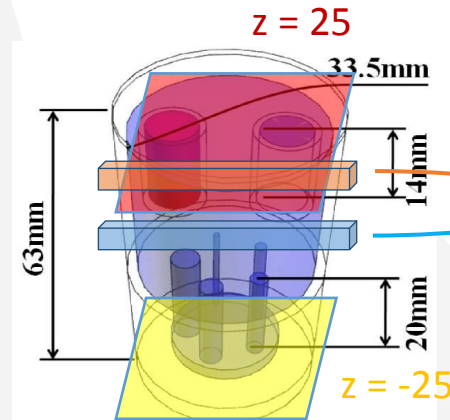
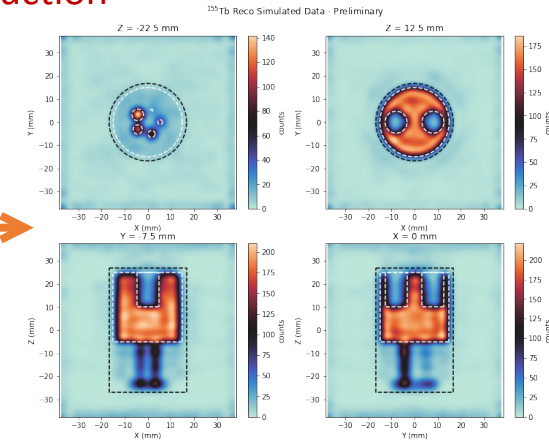
² NEMA Standards Publication NU 4-2008 Performance Measurements of Small Animal Positron Emission Tomographs National Electrical Manufacturers Association 1300 N. 17th Street, Suite 1752 Rosslyn, VA 22209.

- Monte Carlo simulation: GATE¹ 10 Platform (Geant4 based)
- Tomographic Reconstruction:
 - Ordered Subset Expectation Maximization (OSEM) algorithm, a Faster MLEM variant used for reconstruction.
 - CASToR¹ platform used for reconstruction, camera implemented and parameters optimized within it.
 - Different parameters was optimized.
 - Corrections factors implemented.

a. 2D Projection



b. 3D image reconstruction (OSEM)



¹ David Sarrut et al 2021 Phys. Med. Biol. 66 10TR03.

² CASToR: a generic data organization and processing code framework for multi-modal and multi-dimensional tomographic reconstruction, Thibaut Merlin et al., 2018.

- Experiments: 3 experiments at CHUV, Lausanne for simulation calibration:
 - 7 MBq of ^{155}Tb ($T_{1/2}$: 5.32 d) phantom (12 h acquisition) – Produced by MEDICIS/CERN .
 - 32.4 MBq (~89%-8%) ^{155}Tb - ^{156}Tb phantom (12 h acquisition) – Produced by PSI. (+3% ^{154}Tb)
 - 50 MBq of ^{161}Tb phantom (4 h acquisition) – Produced by PSI.

Isotope	Half life
^{154}Tb	21.5 h
^{155}Tb	5.32 d
^{156}Tb	5.35 d
^{161}Tb	6.96 d

- To quantify the reconstructed images, multiple factors were calculated:

- Integral uniformity [%]:

$$IU = \frac{\sigma_N}{\bar{N}}$$

σ_N : Standard deviation of voxels values in ROI.
 \bar{N} : Sum of counts in ROI averaged by # of voxels.

- Signal to noise ratio:

$$SNR = \frac{|N_s - N_n|}{N_n}$$

N_s : # of counts considered as signal in ROI.
 N_n : # of counts considered as noise in ROI.

- Contrast factor of the cold cylinders [%]:

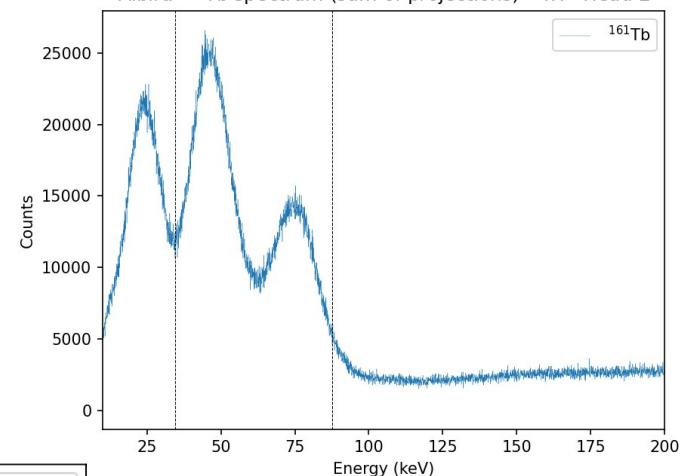
$$Q_{cold} = [1 - \frac{\bar{S}_{cold}}{\bar{S}_{Phantom}}]$$

\bar{S}_{cold} : average counts in the cold cylinder.
 $\bar{S}_{Phantom}$: average counts in the ROI of the phantom.

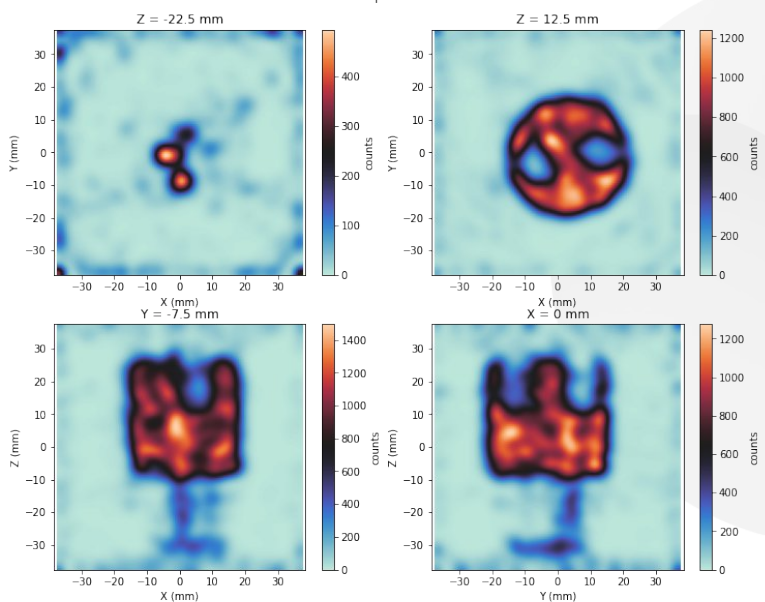
- 2 γ peaks (48.9 keV, 74.6 keV) utilizable for SPECT tomographic reconstruction.
- Despite the notable in-homogeneity & non negligible BG, largest rods well-reconstructed.

➔ Strong potential of ^{161}Tb in imaging clinical application.

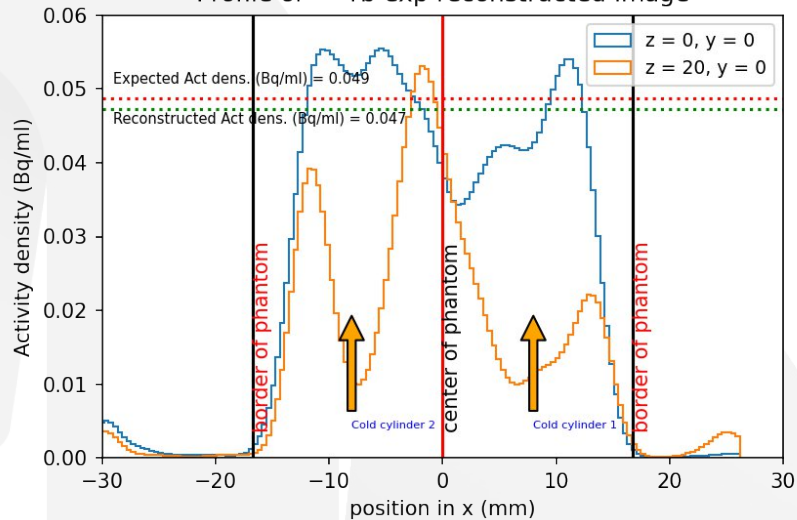
Albira ^{161}Tb spectrum (sum of projections) - 4H - Head 2



^{161}Tb Reco Exp Data - Corrected



Profile of ^{161}Tb exp reconstructed image



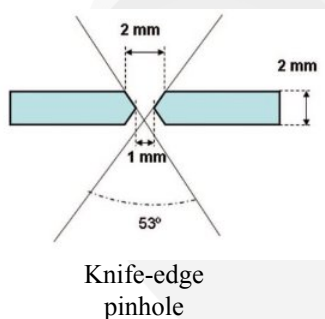
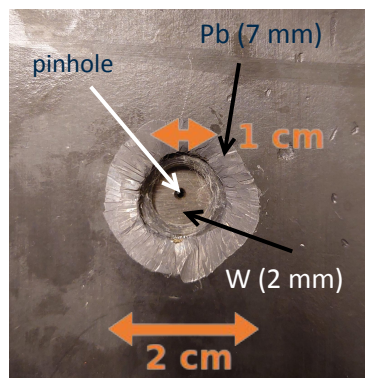
Quantification factor	^{161}Tb Pure
SNR	104.5
IU (%)	16.31
Q_{cold} (%)	88.97

Quant. factor	^{155}Tb exp	^{154}Tb - ^{155}Tb - ^{156}Tb exp
SNR	50.86	7.12
IU (%)	8.39	7.54
Q_{cold} (%)	84.48	63.19

→ ~ 7 times better

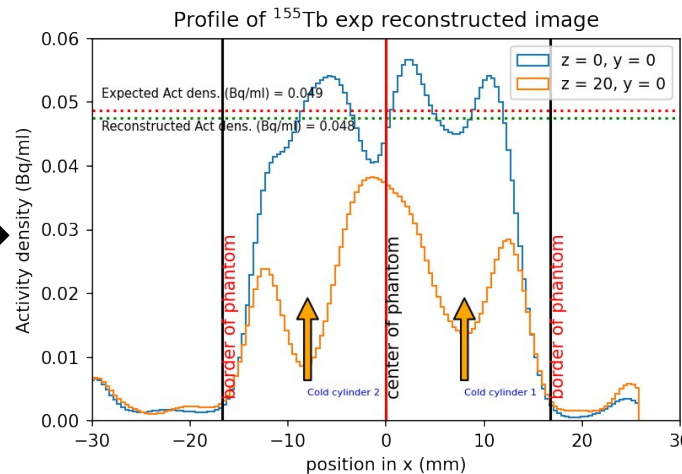
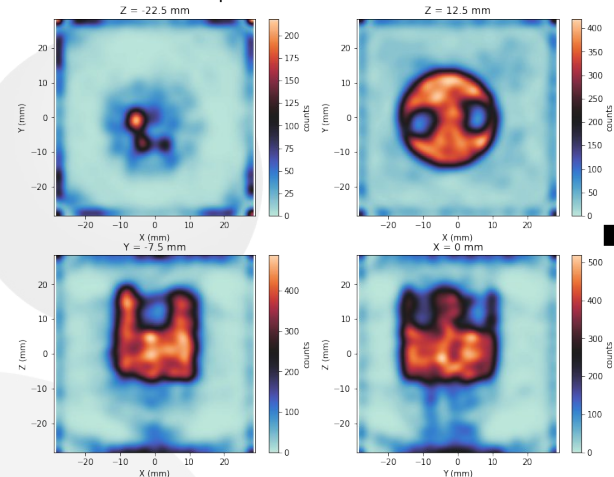
- Image immensely polluted with ^{156}Tb .

→ Shielding and collimation not adapted for these high energies.

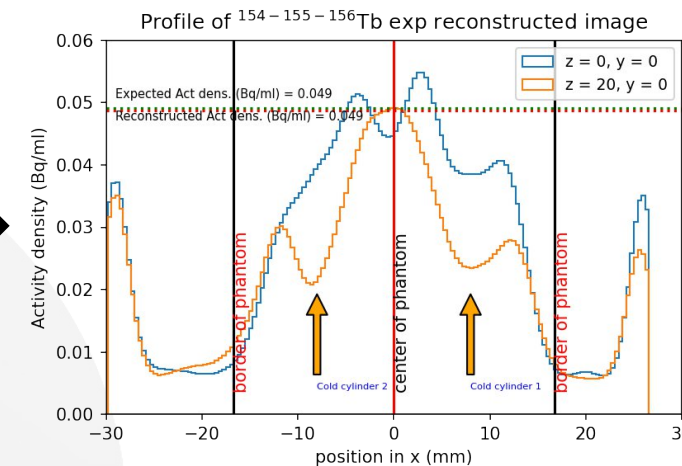
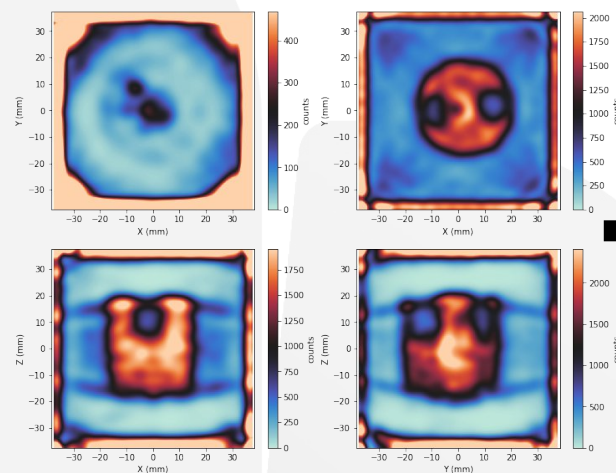


→ To study it using simulation.

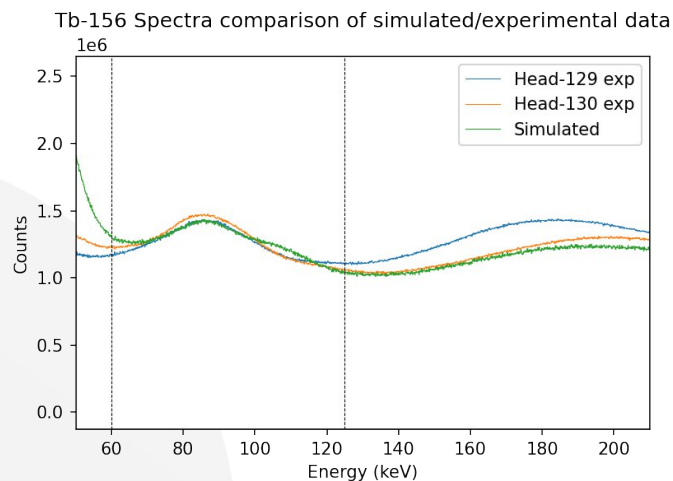
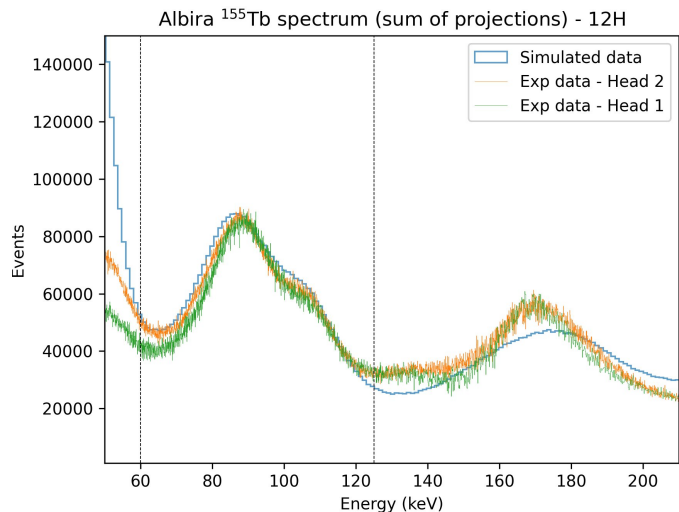
^{155}Tb Reco Exp Data - subtracted and corrected



^{154}Tb - ^{155}Tb - ^{156}Tb Reco Exp Data



- Objectives of simulation:
 - Accurately replicate Albira and validate the simulation based on experimental data.
 - Determine contamination acceptable limit.
 - Optimize collimation and shielding.
 - Methodology:
 - GATE 10 simulation¹ (reproduction) of camera, phantom and all sources (isotopes and contaminants).
 - Simulate different mixtures of isotopes.
 - Simulated spectrum approximately reproduce the experimental one in [50, 200] keV.
- Reproduction of the camera within ROI [60, 125] keV.



- Simulation reconstructed images are more homogeneous, rods ~ 2 mm SR.
- Successful reproduction of the camera output and effective reconstruction.
- Diffusion at borders of phantom even for simulated data > Reco. effect, scattering?

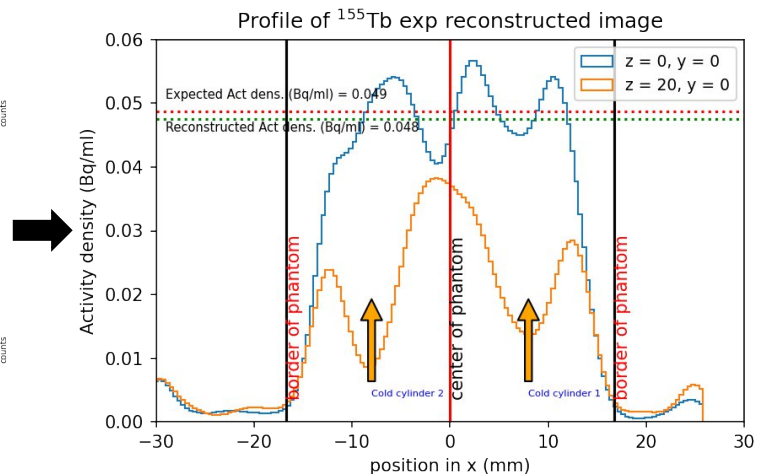
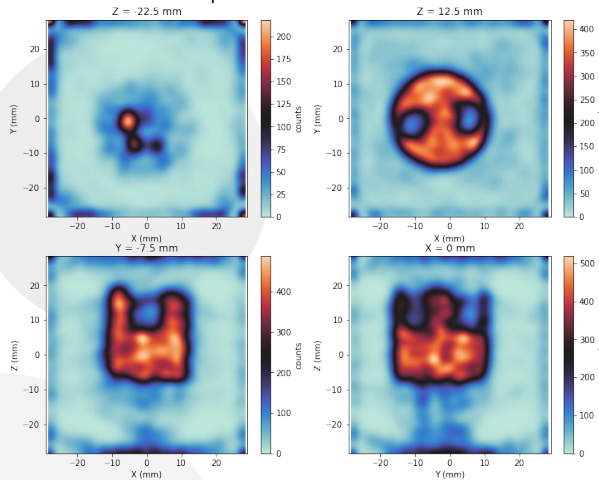
➤ Profiles show that this SPECT camera is not perfectly reproduced by simulation.

Quantification factor	^{155}Tb simu	^{155}Tb exp
SNR	103.9	50.86
IU (%)	4.49	8.39
Q_{cold} (%)	89.73	84.48

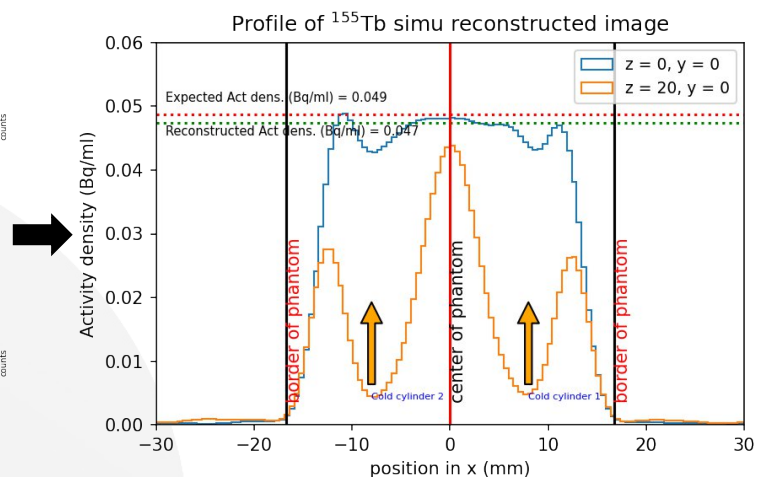
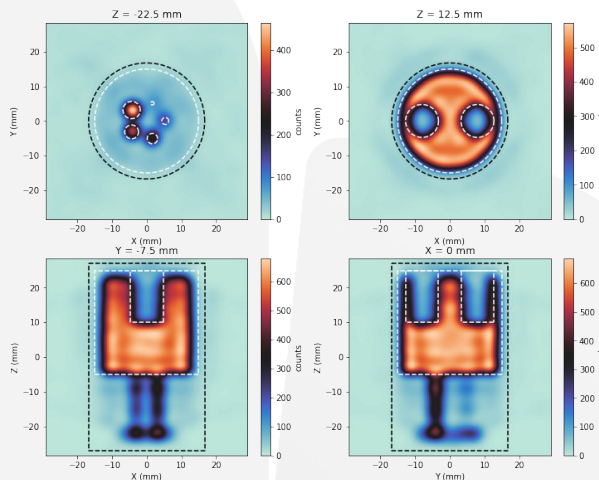
→ >2 times better

→ ~ 2 times better

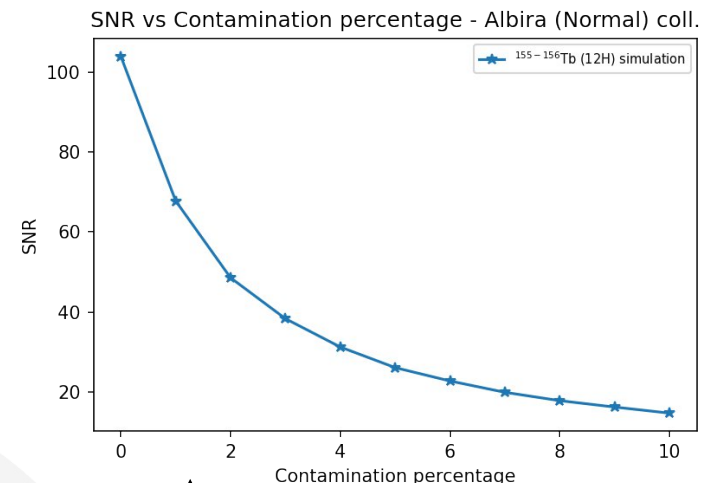
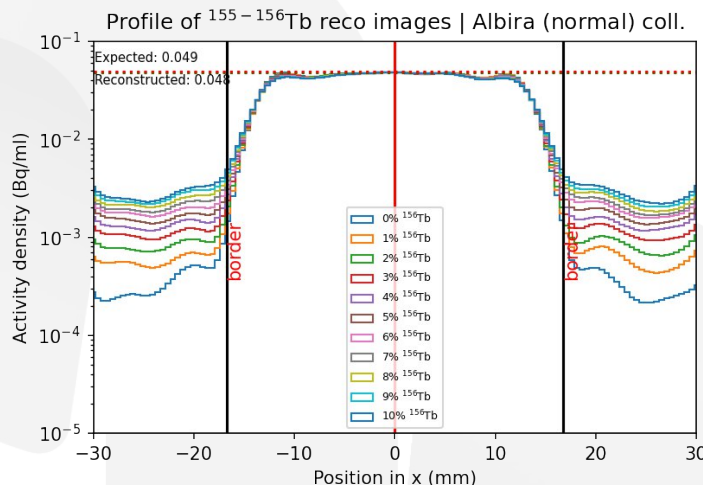
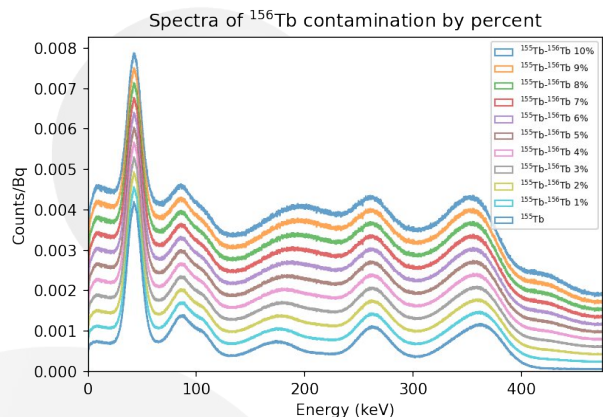
^{155}Tb Reco Exp Data - subtracted and corrected



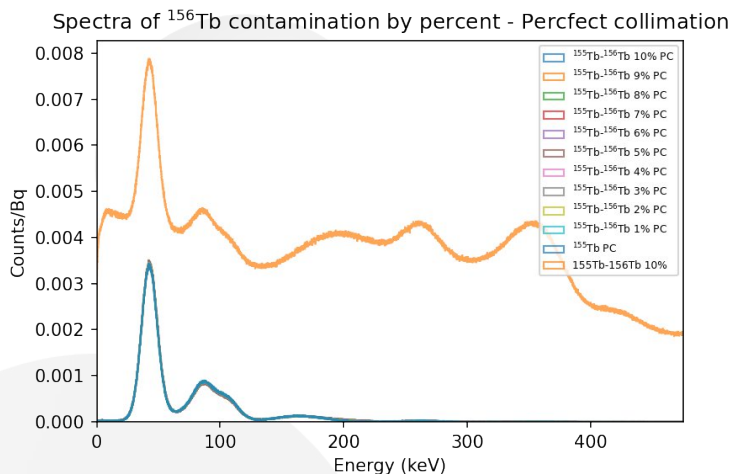
^{155}Tb Reco Simulated Data



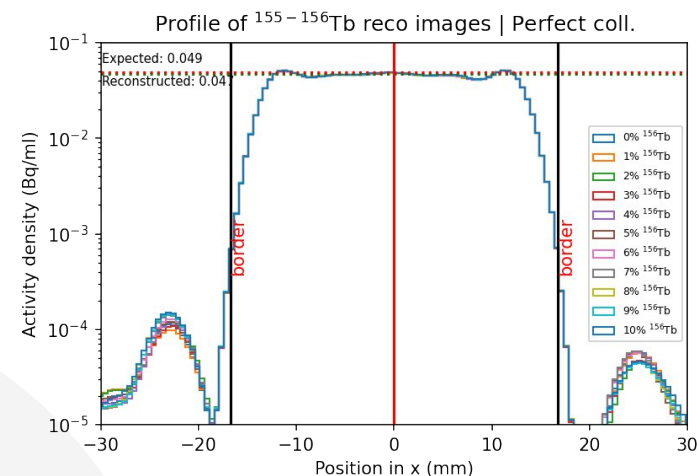
- To study the impact of contamination: ^{155}Tb with ^{156}Tb contamination from 0% to 10% was simulated.
- At 2% ^{156}Tb contamination, SNR drop (exponentially) to its half.
- ^{156}Tb detected counts contribution in ROI:
 - At 1% activity cont. = 25.8%
 - At 10% activity cont. = 79.3%



- To study the impact of low collimator thickness & weak shielding: density of collimator and shielding is set into infinity in the **simulation**.
- Notably ^{156}Tb contribution is negligible if HE collimator is used.
 - Results are not dependent on the radionuclide alone; it depends on the specific imaging camera used.



- ^{156}Tb detected counts contribution in ROI:
 - At 1% activity cont. = 0.5% detected counts
 - At 10% activity cont. = 4.9%



- SPECT camera (Albira) was calibrated, studied and implemented in CASToR.
 - Camera has good performance at low energy, however, high energy gammas are not collimated.
- Experiments of ^{161}Tb , ^{155}Tb & $^{155-156}\text{Tb}$ were performed.
 - Strong ^{156}Tb contamination due to insufficient collimation.
 - ^{161}Tb and (pure) ^{155}Tb projections reconstructed and quantified → confirm imaging capability.
 - ^{161}Tb has strong potential in imaging clinical application.
- Preliminary simulation of MC digital twin of this SPECT camera were done.
- Contamination acceptable limit is dependent on used instrumentation (camera and collimation).
- A well-collimated camera effectively addresses imagery requirements, while dosimetry questions remain under investigation.

- Determine acceptable contamination limit of ^{156}Tb (as a function of collimation) for clinical purposes using simulation.
- Study dosimetric aspects of ^{156}Tb contamination.
- Determine acceptable contamination limit with well-collimated medium energy camera (THIDOS¹).

(1) Medium energy camera developed in our group, optimized at 370 keV.



Thank You

Thank to PRISMAP¹ European project and CNRS MITI, this project was financed by them.

Thanks to C. Duchemin^a, N. van der Meulen^b, Z. Talip^b

1: This project has received funding from the European Union's Horizon 2020 research and innovation programme under grant agreement No 101008571 (PRISMAP)

a: MEDICIS, CERN.

b: Paul Scherrer Institute PSI.

➤ To quantify the reconstructed images, multiple factors were calculated:

- Integral uniformity (IU) [%]:

$$IU = \frac{\sigma_N}{\bar{N}}$$

σ_N : Standard deviation of voxels values in ROI.
 \bar{N} : Sum of counts in ROI averaged by # of voxels.

- Signal to noise ratio (SNR):

$$SNR = \frac{|N_s - N_n|}{N_n}$$

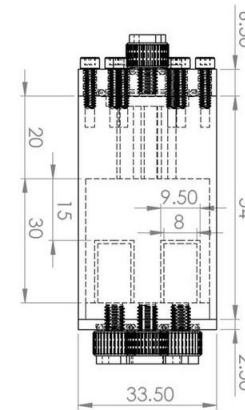
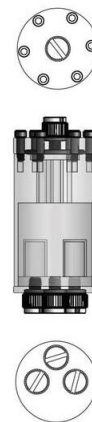
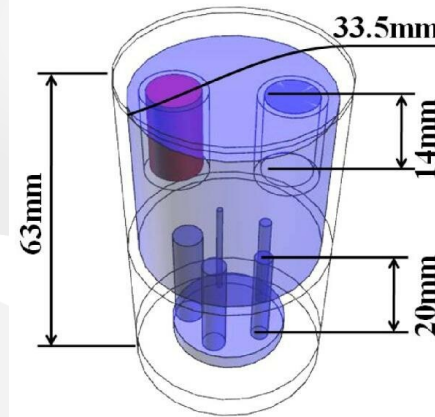
N_s : # of counts considered as signal in ROI.
 N_n : # of counts considered as noise in ROI.

- Contrast factor of the cold cylinders (Q_{cold}) [%]:

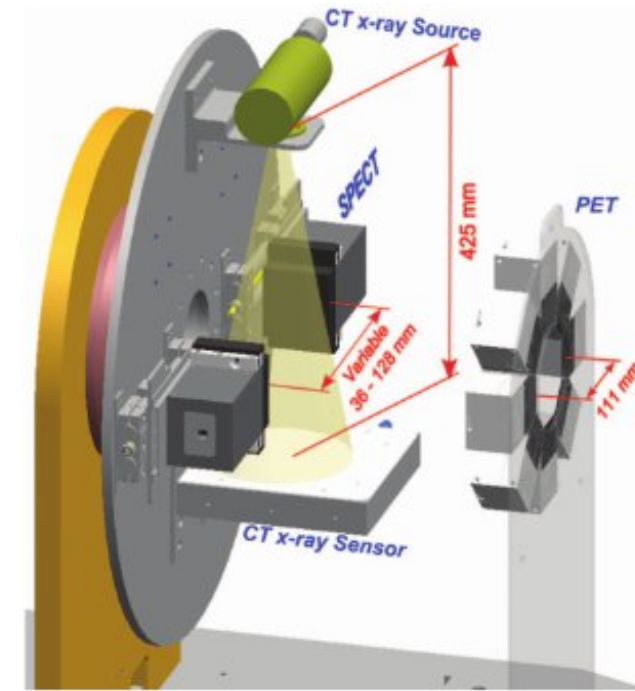
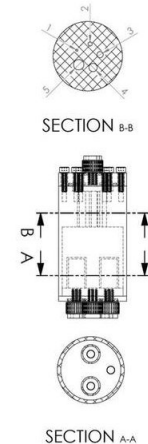
$$Q_{cold} = \left[1 - \frac{\bar{S}_{cold}}{\bar{S}_{Phantom}} \right]$$

\bar{S}_{cold} : average counts in the cold cylinder.
 $\bar{S}_{Phantom}$: average counts in the ROI of the phantom.

- Detector: ALBIRA S108 small animal PET/SPECT/CT (industrial) imaging system (BRUKER)¹.
- 2 rotating SPECT heads, 30 positions/camera (6°).
 - Camera optimized for ^{99m}Tc (140 keV).
 - Single pinhole collimator (2 mm W).
 - Energy range 30-400 keV (BRUKER).
 - Energy Res. (FWHM) : 13.5% @140 keV (BRUKER).
 - Spatial Res.(FWHM) : ~1.5 mm (BRUKER).
 - Projection image in-uniformity.
- Tomo-Reconstruction program implemented.
- Offer access to List-mode data (x,y,E) for each projection.
- Phantom: NEMA NU 4-2008 phantom².
- Study and understand camera performance.



Drawings and dimensions (units in mm)



¹ Sánchez et al. Med. Phys, 40, No. 5, May 2013.

² NEMA Standards Publication NU 4-2008 Performance Measurements of Small Animal Positron Emission Tomographs National Electrical Manufacturers Association 1300 N. 17th Street, Suite 1752 Rosslyn, VA 22209.

- Background studying → count rate 30-40 cps (negligible).
 - Sensitivity disparity between the two heads + geometrical effect → corrected for each projection.
 - Sensitivity drop below ~ 50 keV, and above ~ 200 keV.
 - Measured spatial resolution : 17% at 140 keV.
 - New calibration, calibration of head 1 is non-linear → Complicate treatment and analysis !
 - Projection image non-uniformity cause artifacts in reco images and lower SNR ! → Corrected.
 - Very thin collimator : 2 mm W with pinhole → septal penetration.
 - Shielding adapted for < 140 keV: 6 mm Pb behind collimator and 2 mm on camera sides → high potential scattering.
- An external reconstruction performed to include all these corrections.