BTML 2013 13 septembre 2013





High flux Compact Compton X-ray Sources ThomX, a demonstrator

Marie Jacquet

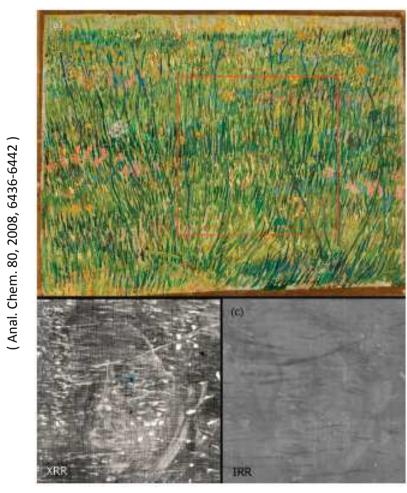
Laboratoire de l'Accélérateur Linéaire Orsay, France (IN2P3,CNRS)

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▶ In many scientific domains synchrotron sources are currently the only machines in term of brightness to perform and carry out the most ambitious analyses and searches requiring ~ 10-100 KeV X-rays.

Vincent van Gogh "Un coin d'herbe" (1887) at synchrotron DESY

Conventional X Radiography & IR Reflectography



X Transmission

IR Reflectography

Vincent van Gogh "Un coin d'herbe" (1887) at synchrotron DESY

Conventional X Radiography & IR Reflectography



X Transmission

IR Reflectography

Analyses at synchrotron DESY (non destructive)

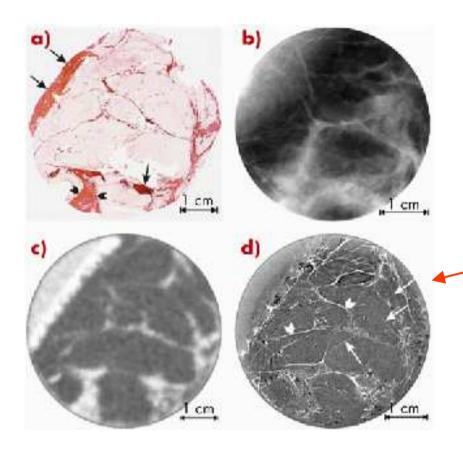
Colored reconstruction



(Anal. Chem. 80, 2008, 6436-6442)

Biomedical: imaging human breast tissue at synchrotron ESRF

Mapping of a breast tissue sample



(Phys. Med. Biol. 52, 2007, 2197-2211)

- a) Histological section(used as a standard for interpretation)
- b) Clinical planar screen-film mammogram taken at the hospital
- c) Clinical scanner
- d) ID17 ESRF (Phase constrast imaging)Same dose as c)

Stronger contrast

→ Improvement in the visualisation of the morphology and of the overall architecture of the breast tissues

- ► In many scientific domains synchrotron sources are currently the only machines in term of brightness to perform and carry out the most ambitious analyses and searches requiring ~ 10-100 KeV X-rays.
- ► Compact lab sources today does not allow to carry out many of the techniques used at synchrotrons.

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<u>X-ray tubes</u>: The most efficient are rotating anodes (Rigaku \sim 10^{10} ph/sec, polychromatic)
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Synchrotron sources are very powerful, but,

- not very "pratical" for some applications,
- with a limited access time.
 - → Developing intense lab sources should avoid these limitations
- Compact Compton Sources (CCS)

Methods currently used at synchrotrons and requiring a high brightness beam could be largely developed in a lab size environment (hospitals, labs, museums).

- Compactness (surface ~ 100 m²)
- High intensity (1012 1014 ph/sec)
- Tunable beam
- High quality beam (brightness 10¹¹ 10¹⁵ ph/sec/ mm² / 0.1% bw / mrad²)

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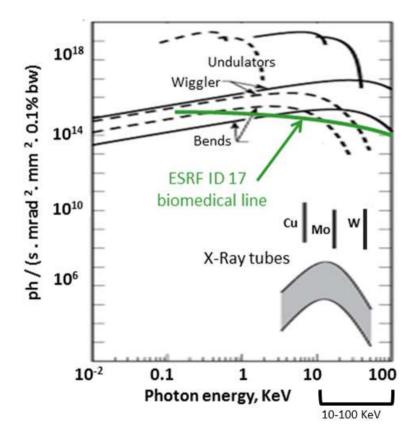
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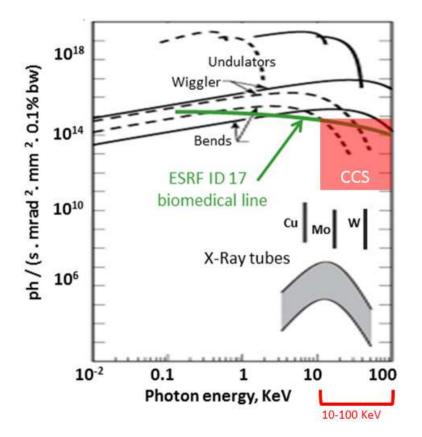
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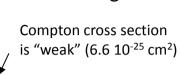
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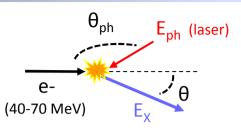
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X-ray Compton Sources: principle and specifications

Compton scattering where the electron is no longer at rest

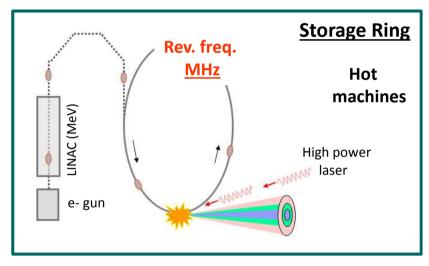


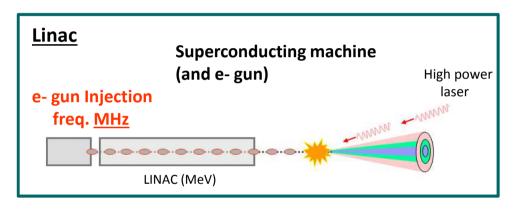


$$E_{X} \sim \frac{2 \gamma^2 E_{ph} [1 - \cos(\theta_{ph})]}{1 + (\gamma \theta)^2}$$

$$\gamma = E_e / m_e >> 1$$
$$E_{ph} << m_e$$

1. <u>High flux</u> $(10^{12} - 10^{14} \, \text{ph/sec}) \rightarrow \text{Increase } f_{\text{rep}} \text{ e}^{\text{-}/\text{laser}} \ (^{\sim} 10\text{-}100 \, \text{MHz}) \rightarrow 2 \, \text{main schemes}$

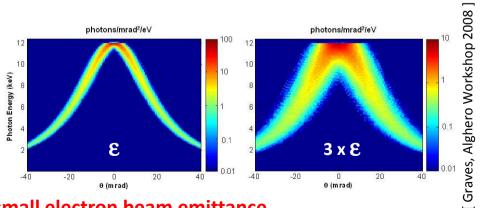




2. High brightness $(10^{11} - 10^{15})$

Br ~
$$\frac{\text{Flux}}{(\text{mm}^2 \text{ source}) (\text{dE}_x/\text{E}_x) (\text{mrad})^2} \sim \frac{\text{Flux} \cdot \gamma^2}{\epsilon_N^2}$$

 $\sigma_e^2 \sigma_e'^2 = \epsilon^2$

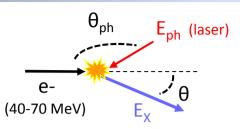


→ small electron beam emittance

X-ray Compton Sources: principle and specifications

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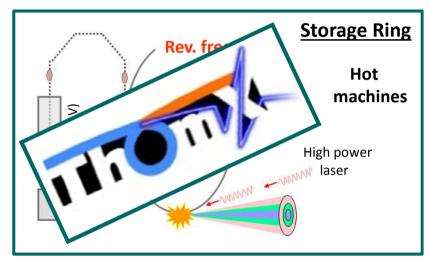
> Compton cross section is "weak" (6.6 10⁻²⁵ cm²)

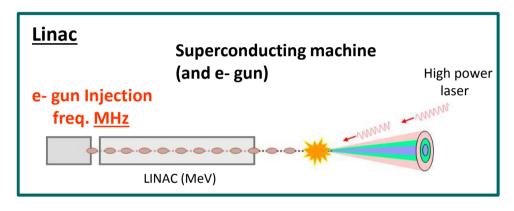


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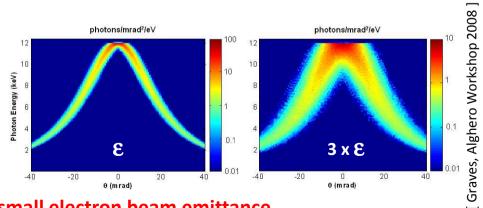




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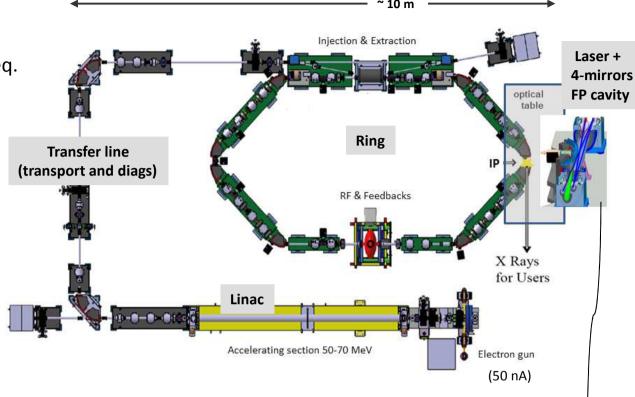
ThomX design



Electron machine

- 1 nc / bunch , 50 Hz inj. freq.
- Ring, 20 MHz frep.
- $\sigma_e \sim 70 \, \mu m$
- $\varepsilon_N \sim 4 \text{ mm.mrad}$
- $\tau_e \sim 10\text{-}20 \text{ ps}$

Machine funded In construction

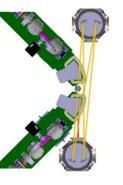


X-ray beam

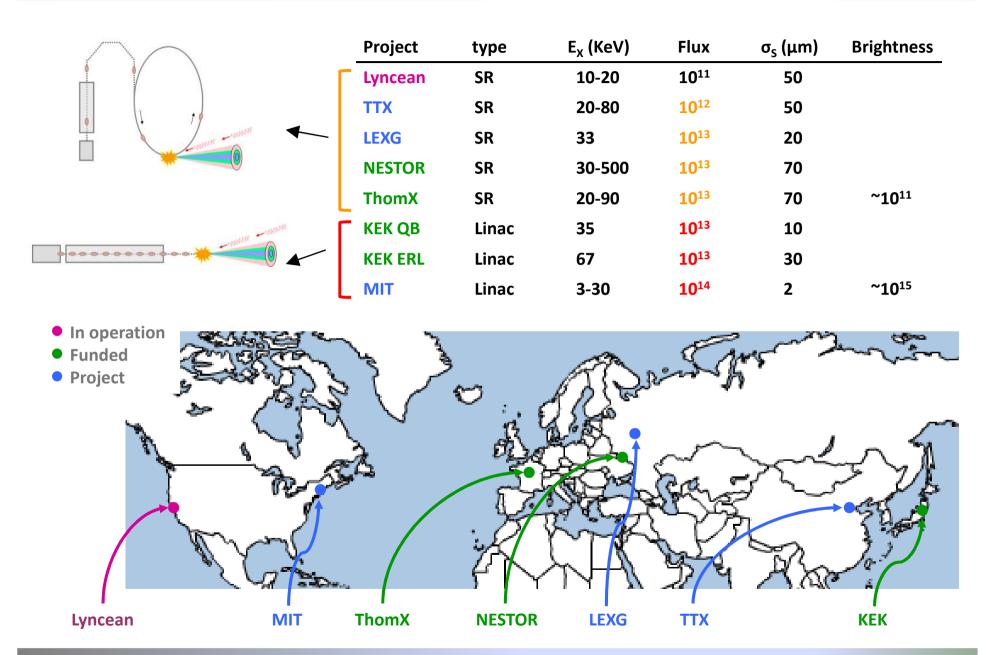
•	
Flux	10 ¹³
Brigthness	10 ¹¹
Transv. size	70 μm
E _X	20-90 KeV

Laser / Cavity system

- Laser ~ 1W
- Optical fiber amplification (100 W) 2-3 μJ/pulse
- Optical FP cavity amplification (gain 10000)
- 1 MW stored inside the cavity (20-30 mJ/pulse)



Compact Compton projects (X-ray flux > 10¹² ph/sec)



Compact Compton projects (X-ray flux > 10¹² ph/sec) → Chalenges

	Project	type	E _x (KeV)	Flux	$\sigma_{\rm S}$ (μ m)	Brightness
Achieve the laser/cavity	Lyncean	SR	10-20	10 ¹¹	50	
system requirements \leftarrow	TTX	SR	20-80	10 ¹²	50	
→ 1 MW stored	LEXG	SR	33	10 ¹³	20	
inside the cavity	NESTOR	SR	30-500	10 ¹³	70	
	ThomX	SR	20-90	10 ¹³	70	~1011
Acquire the control of a	KEK QB	Linac	35	10 ¹³	10	
low energy storage ring	KEK ERL	Linac	67	10 ¹³	30	
→ keep a stable & good quality beam	MIT	Linac	3-30	1014	2	~10 ¹⁵

LINAC scheme machine: 2 main technical challenges

- Construction/validation of a superconducting electron gun delivering bunches with an extremely low emittance and ~ 100 MHz of injection frequency
- Difficulties in radioprotection for integration:

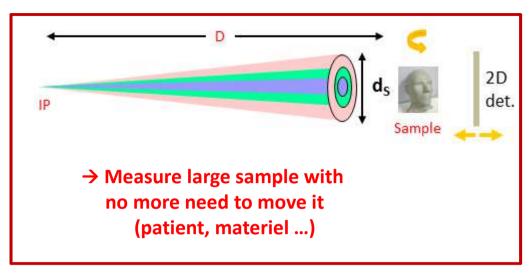
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MIT \rightarrow 0.01 nc / bunch , 100 MHz, 40 MeV \rightarrow 40 KW to be absorbed ThomX \rightarrow 1 nc / bunch , 50 Hz, 50 MeV \rightarrow 2.5 W
```

1. Using the 2D divergent beam

(biomedical and cultural heritage applications)

IMAGING

- Conventional radiography
- K-edge substraction imaging
- Phase contrast imaging
- Magnification
- Radiotherapy

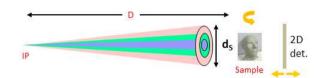


Pink beam (3-30% bw)

1. Using the 2D divergent beam

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- **High energy** (~ 80KeV) to test high-Z element drug
- No need of monochromaticity (pink beam, bw ~ 30%)

Ex. : Human head phantom



- 5 mrad opening angle
- $d_S = 12 \text{ cm} \text{ at D} \sim 15 \text{ m}$
- 6.10¹² ph/s
- bw 60-90 KeV

ThomX and Synchrotron (ID17/ESRF) → comparable

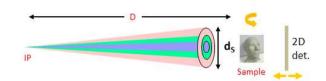
Compared to hospital sources:

- → allow the reduction of the dose
- → better image quality

1. Using the 2D divergent beam

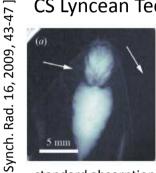
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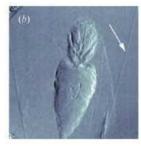
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- bw 2-3%
- Small source size (to have transv. coherence)

CS Lyncean Tech. (only CCS in operation in the word)





13.5 KeV, 3% bw 10⁹ ph/sec σ = 165 μ m

Proof of principle

standard absorption

phase-contrast



- 70 KeV, 2-3% bw, $\sigma \sim 70 \mu m$ $d_S = 4 cm$ at D $\sim 15 m$

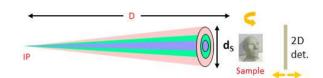
Hospital sources

(large focal spot size, broad spectrum, low flux)

1. Using the 2D divergent beam

(biomedical and cultural heritage applications)

- Conventional radiography
- K-edge substraction imaging
- Phase contrast imaging
- Magnification
- Radiotherapy



- High energy (~ 80KeV)
- bw ~ 10%



- 80 KeV ± 10 KeV
- $d_s = 5 \text{ cm} \text{ at D} \sim 10 \text{ m}$
- 3.10¹² ph/s

Ex.: Human head tumor (tumor deliver dose ~ 10-20 Gy)

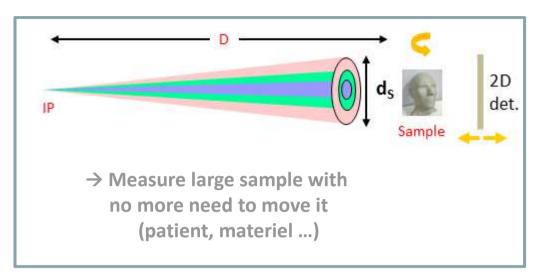
- ThomX → 9 mGy/sec → 20-30 min of irradiation
- **ESRF/ID17** (~ 6 mGy/sec)
- Hospital sources → broad spectrum,
 and continuously operation not possible

1. Using the 2D divergent beam

(biomedical and cultural heritage applications)

IMAGING

- Conventional radiography
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- Phase contrast imaging
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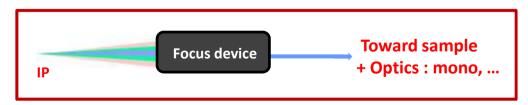


Pink beam (3-30% bw)

2. Using the central part of the beam

(cultural heritage / material science applications)

- Fluorescence Spectroscopy
- XANES Spectroscopy
- Diffraction
 - → Structural analyses
 - → Pump-probe experiments



Quasi-monochromatic beam (~ 1% - 0.01 % bw)

1. Using the 2D divergent beam

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- Conventional radiography
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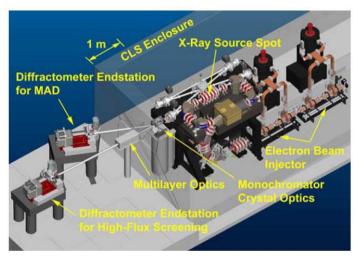
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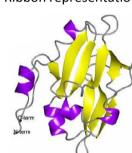
- Quasi-monochromatic beam

1st determination of the 3D structure of a protein CS Lyncean Tech. source



15 KeV, 1.4% bw 5.10^6 ph/sec $\sigma = 120 \mu m$

Ribbon representation



[J. Struct. Funct. Gen. 11, 2010, 91-100]

<u>Proof of principle</u> (~ Rigaku rotating anode)



• 10^9 ph/s , $\Delta E/E \approx 10^{-2} - 10^{-3}$



Conclusions/Outlook

CCS combine

- Compactness
- High flux/brightness
- Tunable energy
- Transverse coherence

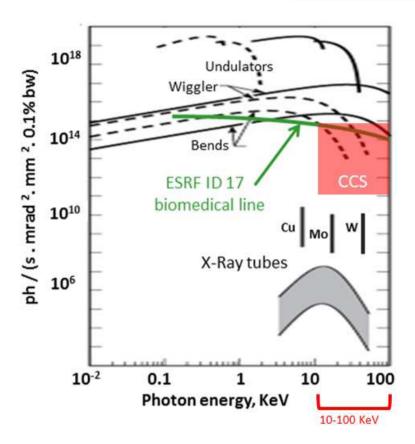
Today

→ Hot machines

- THE STATE OF THE S
- → Brightness ~ 10¹¹

... and tomorrow

- → Supra machines (e- gun)
- \rightarrow Brightness ~ 10^{13} - 10^{15}



CCS will open a new approach in research and development of applications

- Biomedical science
- Cultural heritage research
- Material science

- → Imaging techniques using a large 2D beam = golden applications
- → Fill the great lack of intense lab sources.

