

FRENCH-UKRAINIAN on instrumentation development for high energy physics

1-3 october 2014 LAL-Orsay, France

workshop



ThomX : the instrument and its applications

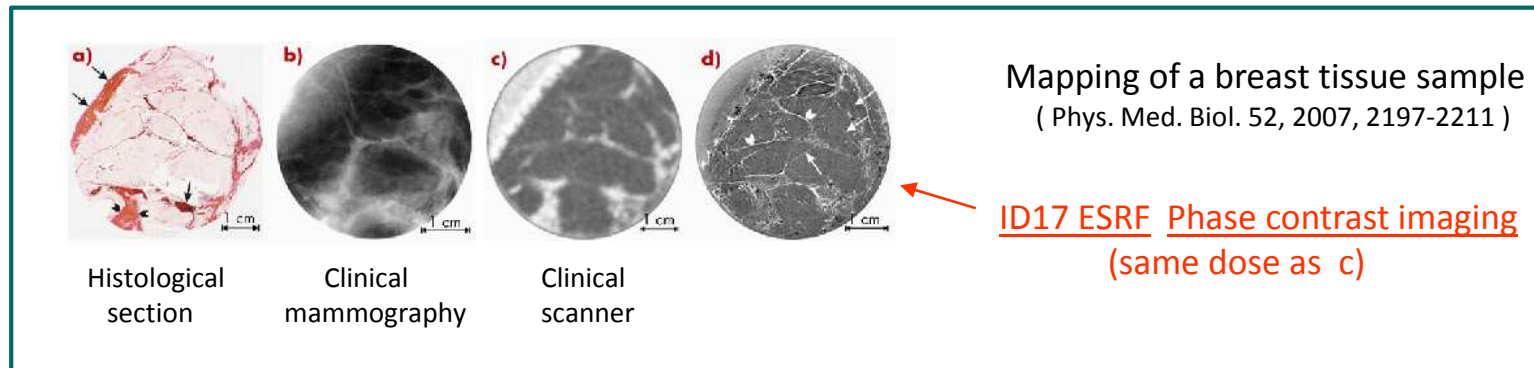
Marie Jacquet
mjacquet@lal.in2p3.fr



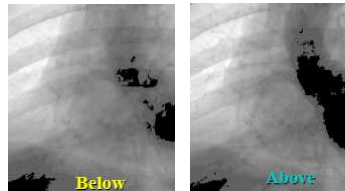
LAL, Orsay, France (IN2P3,CNRS)

Why X-ray users need “compact” X-ray source ?

- ▶ In many scientific domains **synchrotron sources** are currently the only machines in term of brightness to perform and carry out **the most ambitious analyses and searches** requiring **~ 10-100 keV X-rays**.

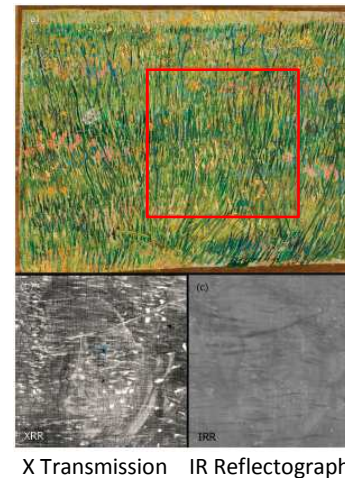


K-edge at ESRF (+contrast agent)



The difference increase the contrast

Vincent van Gogh
“Un coin d’herbe”
(1887)



DESY synchrotron - Fluorescence
- XANES

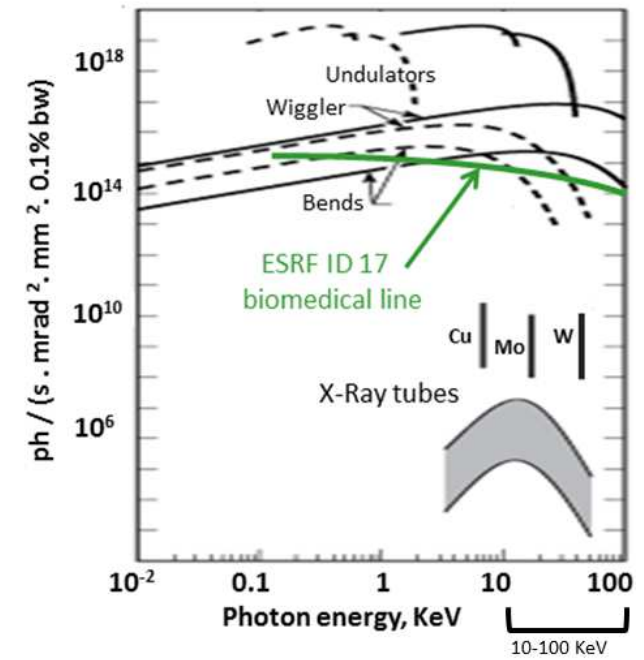


(Anal. Chem. 80, 2008, 6436-6442)

- ▶ Synchrotron sources are very powerful, but :
 - **not very “pratical”** for some applications,
 - **with a limited access time.**

→ **Developing intense lab sources** should avoid these limitations

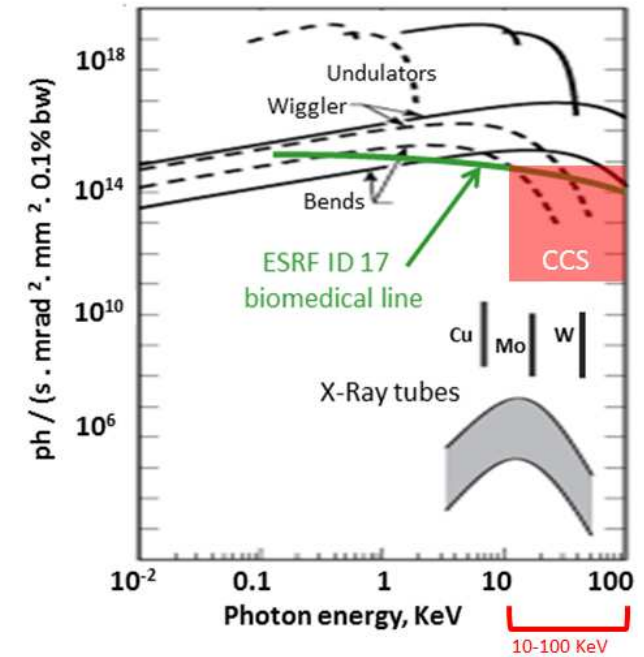
Current panorama of the X-ray source brightnesses



Current panorama of the X-ray source brightnesses

► Compact Compton Sources (CCS)

- **Compactness** (surface $\sim 100 \text{ m}^2$)
- **High intensity** ($10^{12} - 10^{14}$ ph/sec)
- **Tunable beam**
- **High quality beam**
(brightness $10^{11} - 10^{15}$ ph/sec/ $\text{mm}^2 / 0.1\% \text{ bw} / \text{mrad}^2$)



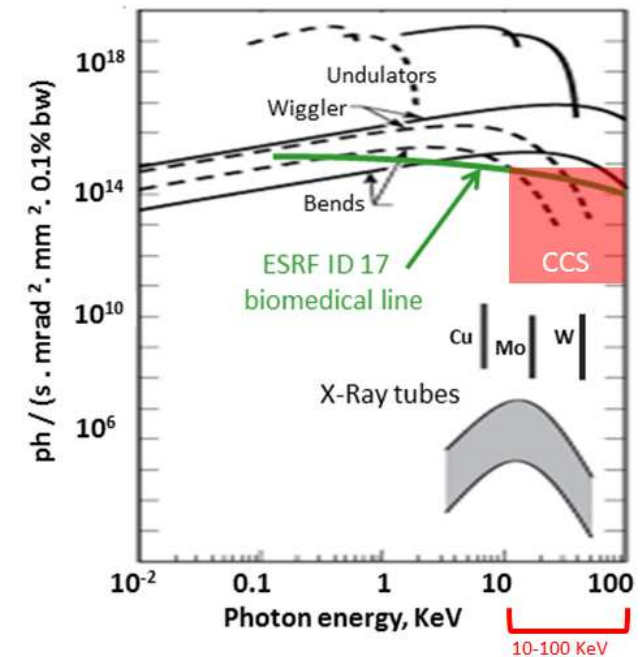
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→ Methods currently used at synchrotrons and requiring a high brightness beam could be largely developed in **a lab size environment** (hospitals, labs, museums).



Compton Sources : principle

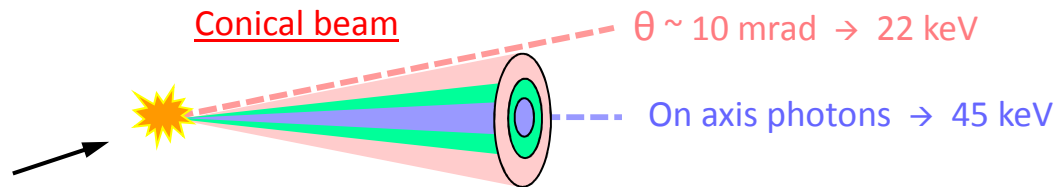
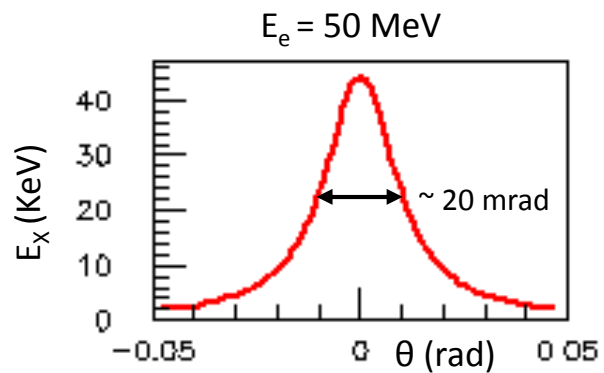
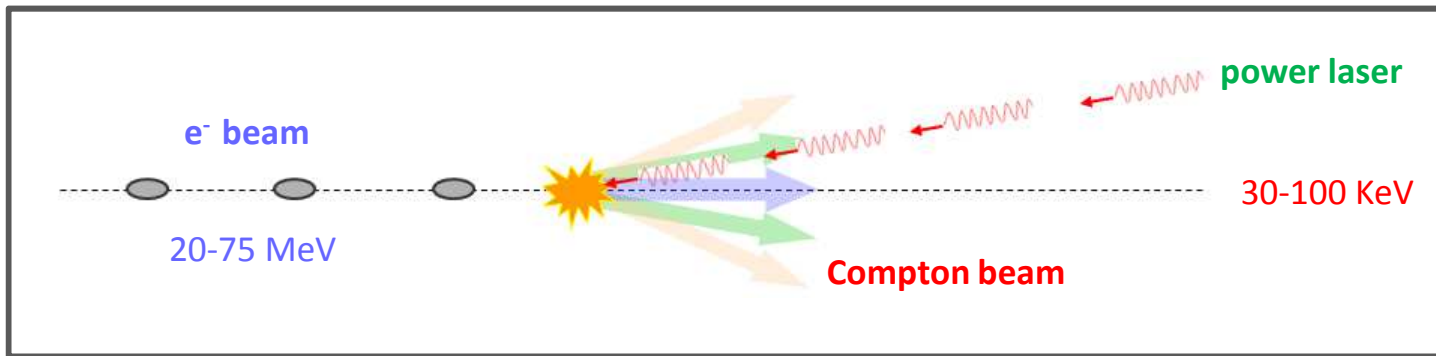
Compton scattering where the electron is no longer at rest



“Inverse Compton” regime

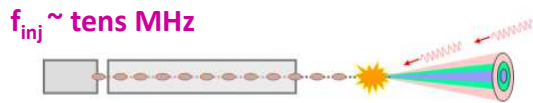
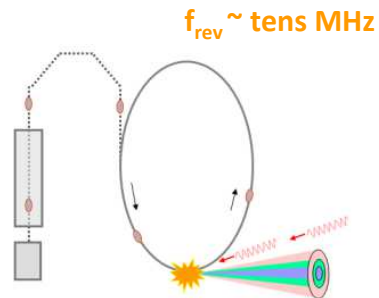
$$E_x \sim \frac{2 \gamma^2 E_{ph} [1 - \cos(\theta_{ph})]}{1 + (\gamma\theta)^2}$$


($\gamma = E_e/m_e \gg 1$; $E_{ph} \ll m_e$)



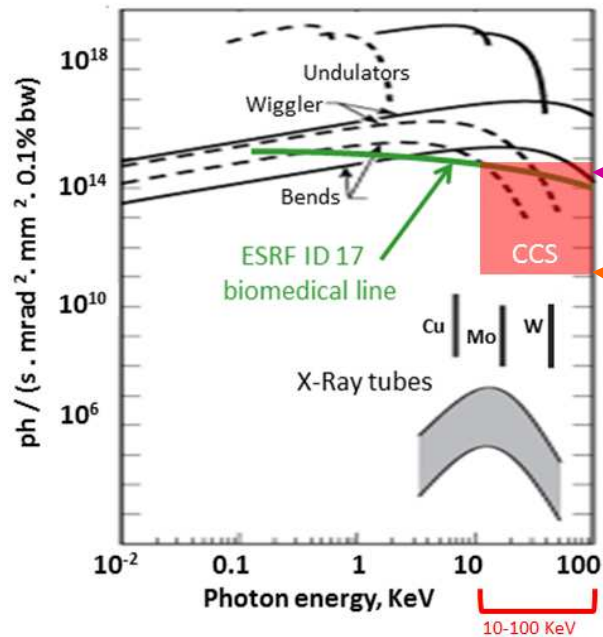
Univocal relation between energy E_x and diffusion angle θ

Compact Compton projects (X-ray flux > 10¹² ph/sec)



Project	type	E _x (KeV)	Flux	σ _s (μm)	Br
* Lyncean	SR	10-20	10 ¹¹	50	
x TTX	SR	20-80	10 ¹²	50	
x LEXG	SR	33	10 ¹³	20	
• NESTOR	SR	30-500	10 ¹³	70	
• 	SR	20-90	10 ¹³	70	~10 ¹¹
• KEK QB	Linac	35	10 ¹³	10	
• KEK ERL	Linac	67	10 ¹³	30	
x MIT	Linac	3-30	10 ¹⁴	2	~10 ¹⁵

* In operation • Funded x Not funded



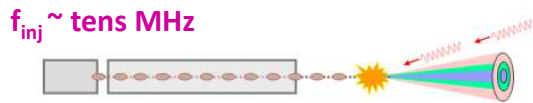
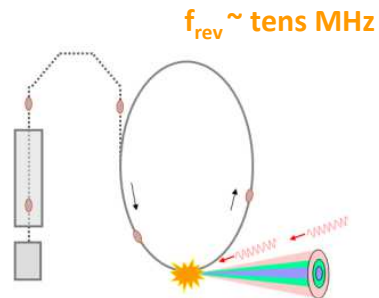
Next future
(supra machines)

Near future
("hot" machines)

Remaining strong challenges:

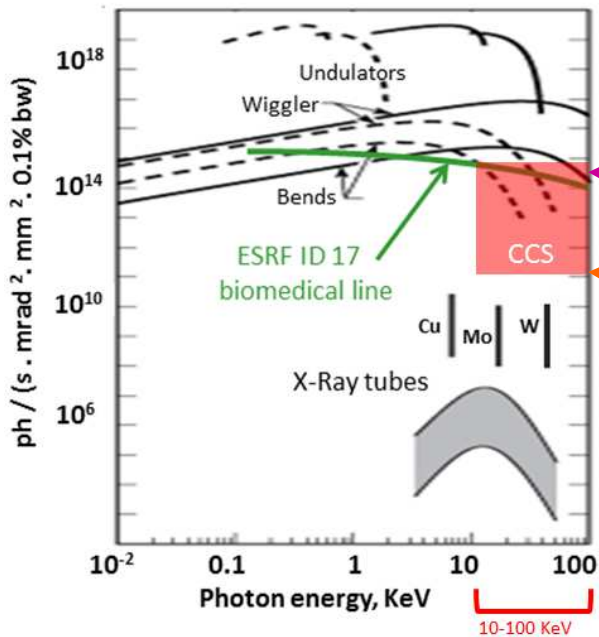
- Supra e-gun : 100 MHz of inj. freq.
ε_N ~ 0.1 mm.mrad
- Radioprotection
 - MIT : 0.01 nc/bunch , 100 MHz , 40 MeV
→ 40 KW to be absorbed
 - ThomX : 1 nc/bunch , 50 Hz , 50 MeV
→ 2.5 W

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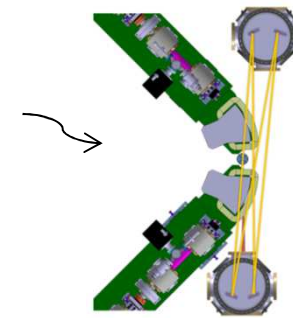
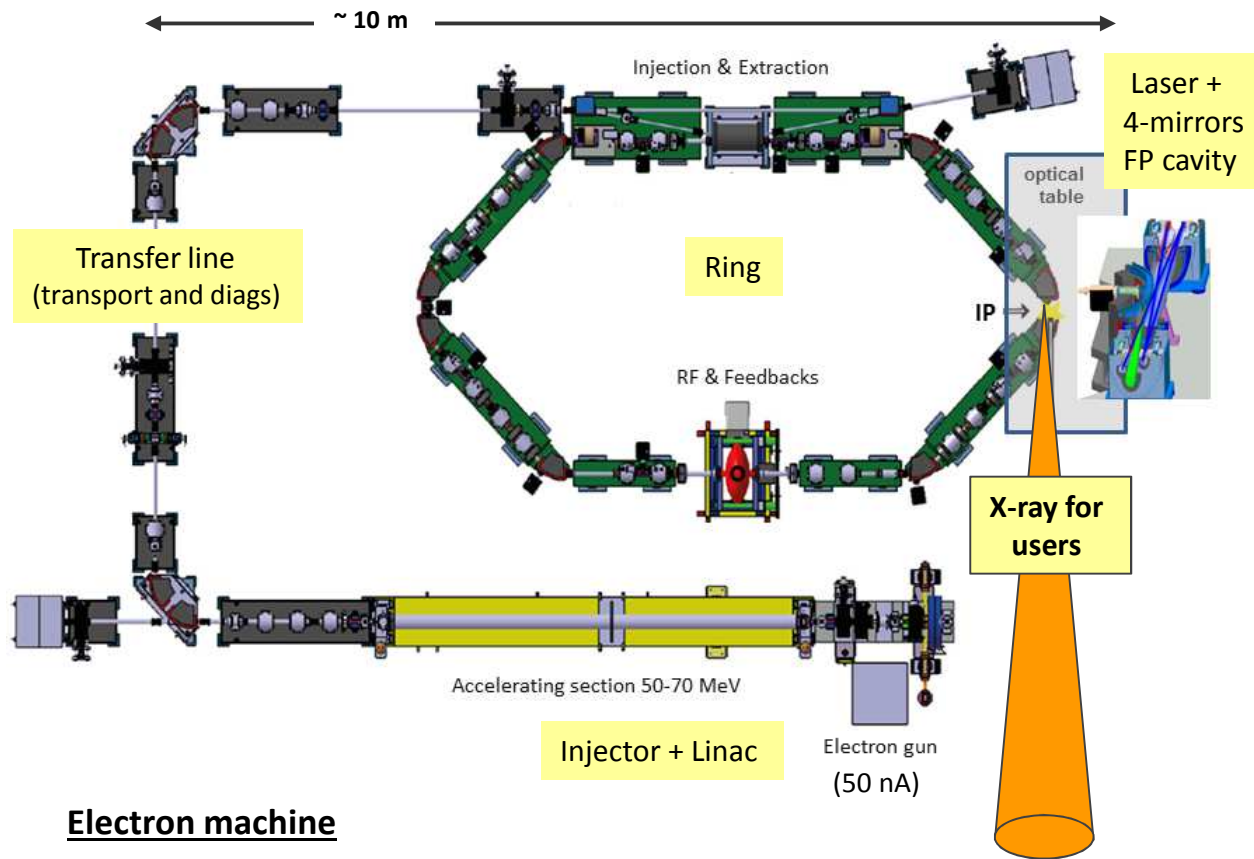


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Laser /Cavity system

- Laser ~ 1W average
- Optical fiber amplification
→ (100 W) 2-3 μJ/pulse
- Optical FP cavity amplification
→ (gain 10000)
- **1 MW stored inside the cavity**
→ (20-30 mJ/pulse)

Electron machine

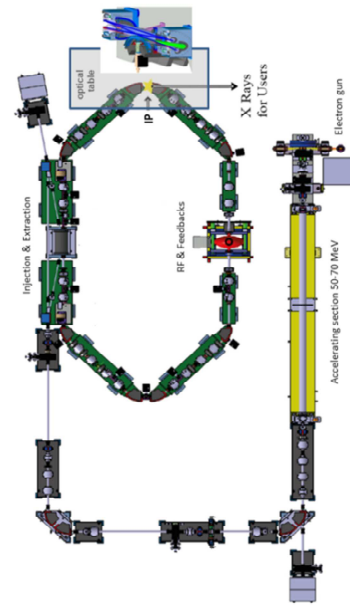
- 1 nc / bunch , 50 Hz inj. freq.
- 50-70 MeV
- Ring, 20 MHz freq.
- $\sigma_e \sim 70 \mu\text{m}$
- $\epsilon_N \sim 4 \text{ mm.mrad}$
- $\tau_e \sim 10\text{-}20 \text{ ps}$

X-ray beam

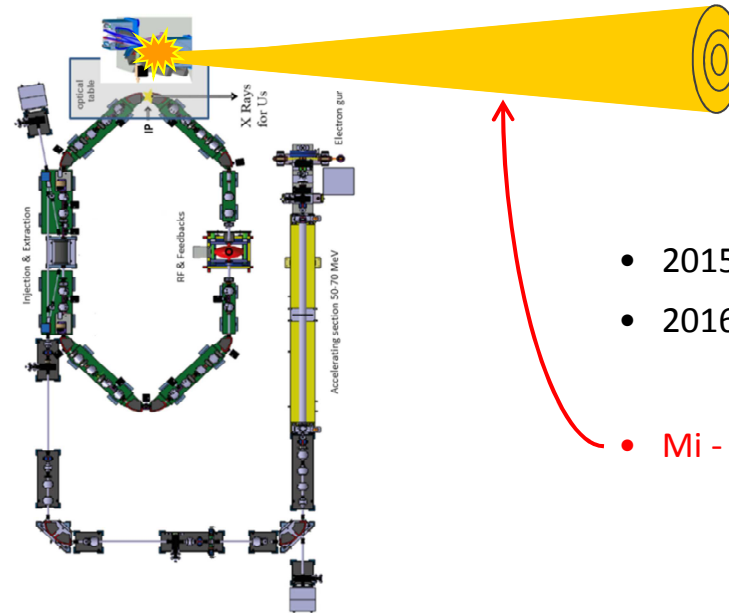
Flux	10^{13}
Brightness	10^{11}
Transv. size	70 μm
E_x	20-90 KeV



Machine funded
In construction



- 2015 - 2016 → Building infrastructure
- 2016 → ThomX installation and commissioning



- 2015 - 2016 → Building infrastructure
- 2016 → ThomX installation and commissioning
- **Mi - 2016**

→ With the first ThomX beam

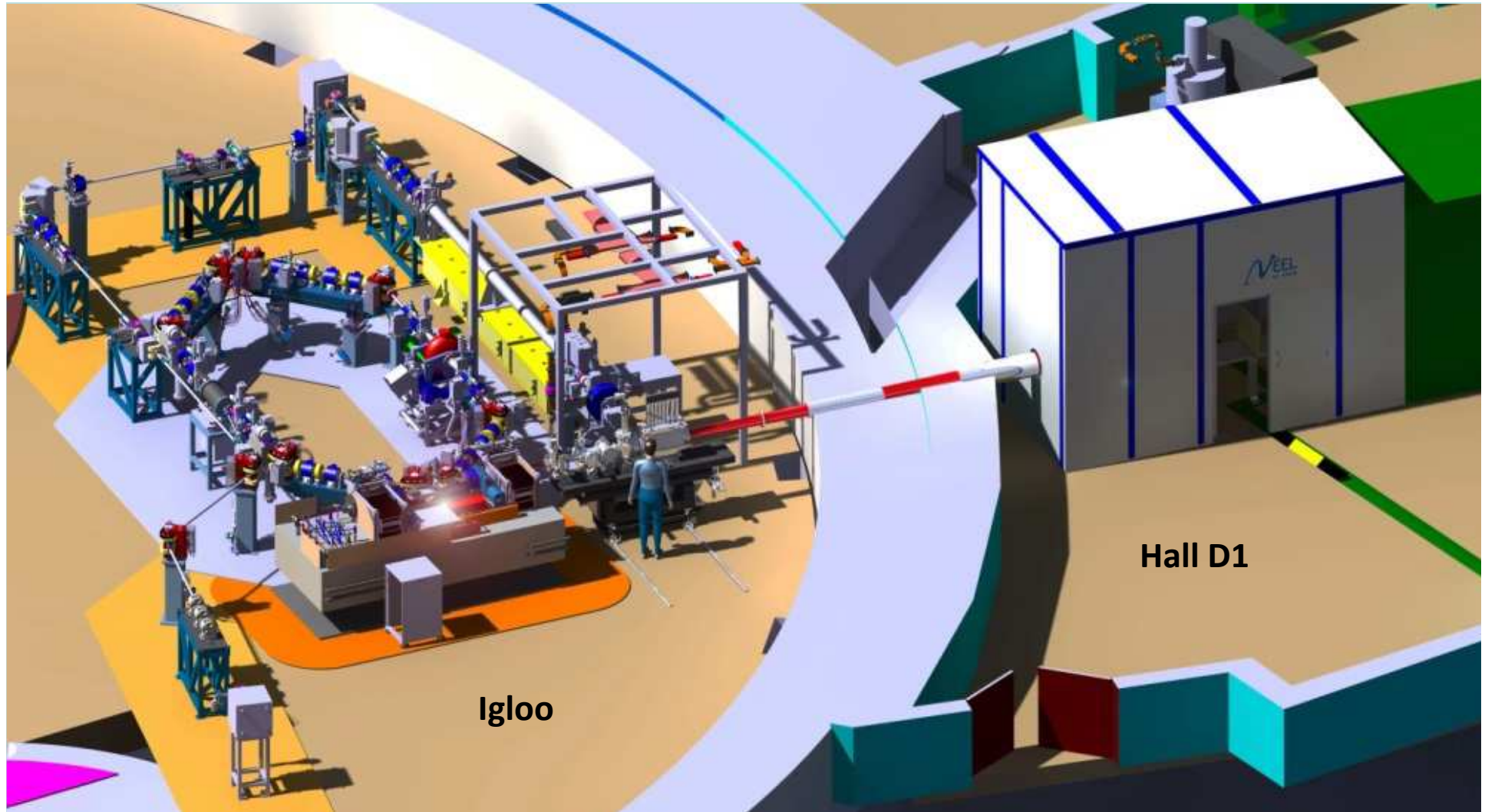
1. Characterization of the Compton beam (spectral flux, source size, energy)
2. Realization of simple demonstration experiments

- Conventional imaging (head phantom)
- K-edge subtraction imaging (head phantom, drugs)
- Phase contrast imaging (nylon wire)
- Radiotherapy (tumor-like mass sample)
- Fluo Spectroscopy
- Diffraction

Biomedical

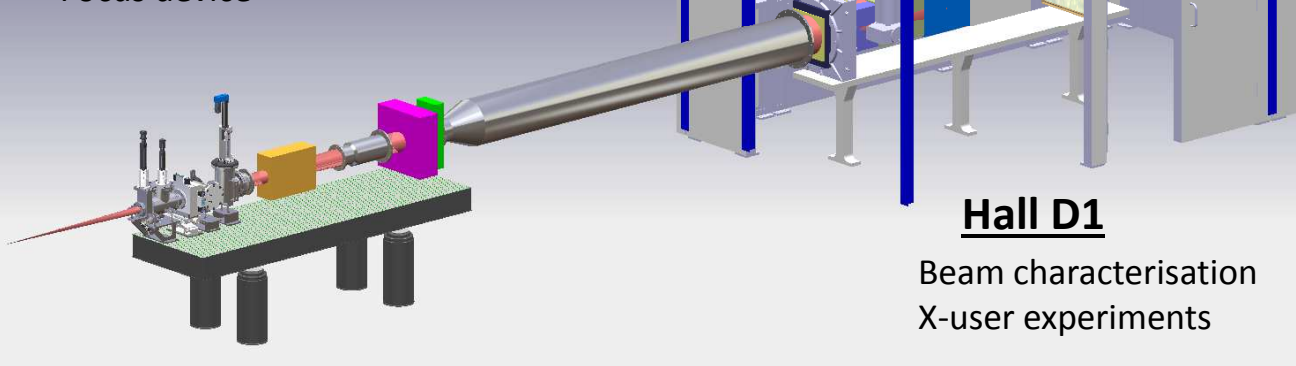
Material science

Techniques where the synchrotron community has already a lot of knowledge and experience



Igloo

Continuous beam monitoring
Focus device

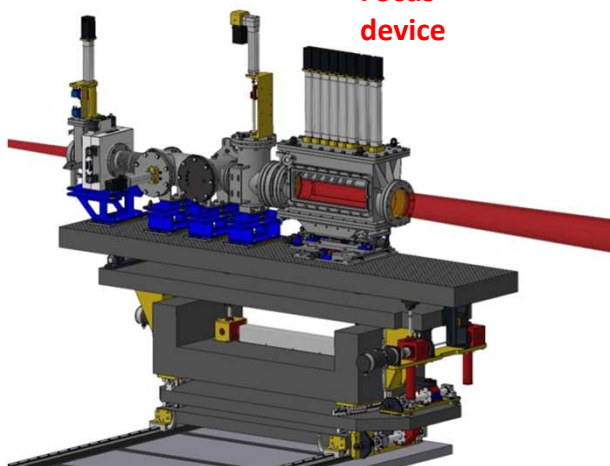


Hall D1

Beam characterisation
X-user experiments

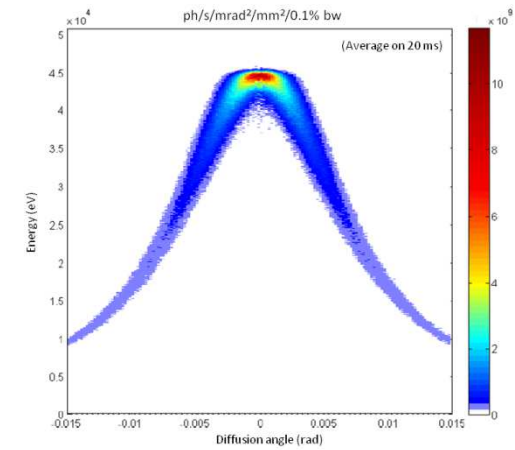
Continuous beam
monitoring

Focus
device



Beam characterisation

1. Mean absolute Flux_{x,y}(E)



2. Bunch to bunch intensity
variations (20 MHz)

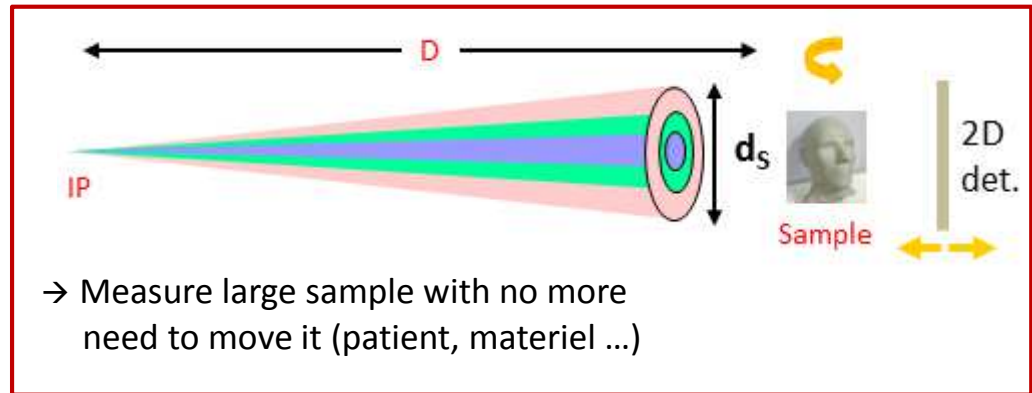
3. Spatial coherence

1. Using the 2D divergent beam

- Conventional radiography
- K-edge subtraction imaging
- Phase contrast imaging
- Radiotherapy

IMAGING

THERAPY



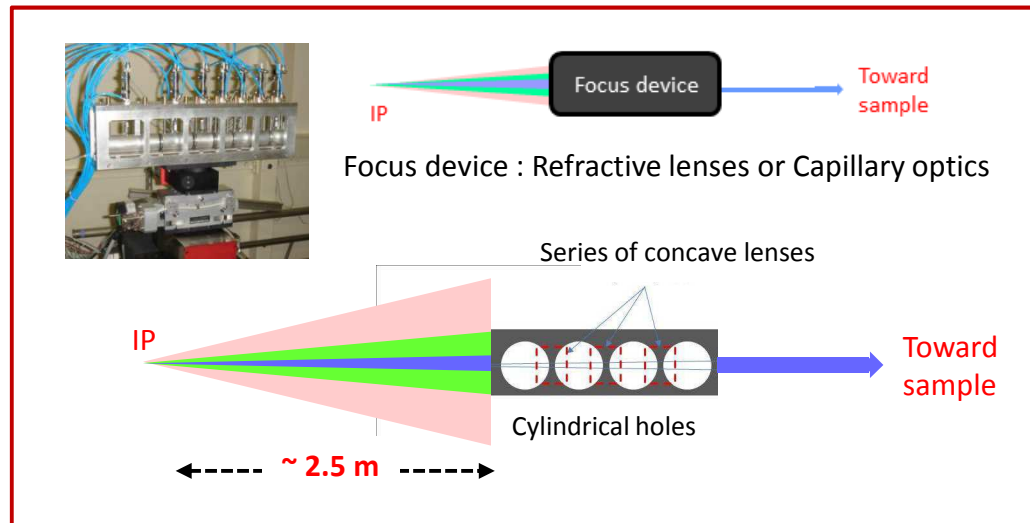
Pink beam $\Delta E/E \sim 3-30\% \text{ bw}$,
several cm diameter, $> 10^{12} \text{ ph/s}$

2. Using the central part of the beam

- Diffraction
- Spectroscopy (fluor, XANES)
- Radiotherapy

MATERIEL SCIENCE

MRT THERAPY ?
(micro/mini beam radiation)



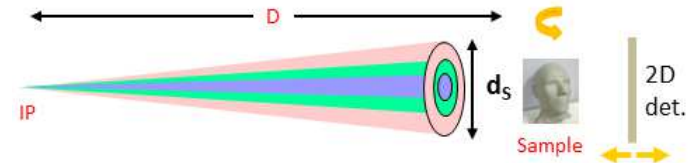
Quasi-monochromatic beam $\Delta E/E \sim 10^{-2} - 10^{-3}$,
mm diameter, $\sim 10^9 \text{ ph/s}$

1. Using the 2D divergent beam

- **Conventional radiography**
- K-edge subtraction imaging
- Phase contrast imaging
- Radiotherapy

IMAGING

THERAPY



- **High energy** ($\sim 80\text{KeV}$) to test high-Z element drug
- No need of monochromaticity (pink beam, bw $\sim 30\%$)



Ex. : Human head phantom radiography

- $d_s = 12\text{ cm}$ at $D \sim 15\text{ m}$
- $6 \cdot 10^{12}\text{ ph/s}$
- bw **60-90 KeV**

2. Using the central part of the beam

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MATERIEL SCIENCE

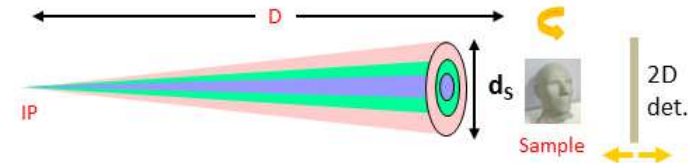
MRT THERAPY ?
(micro/mini beam radiation)

ThomX and Synchrotron (ID17/ESRF) \rightarrow doses comparable
(hospital sources : broad spectrum, low flux)

- \rightarrow reduction of the absorbed dose
- \rightarrow with a better image quality

1. Using the 2D divergent beam

- Conventional radiography
 - K-edge subtraction imaging
 - **Phase contrast imaging**
 - Radiotherapy
- IMAGING
- THERAPY



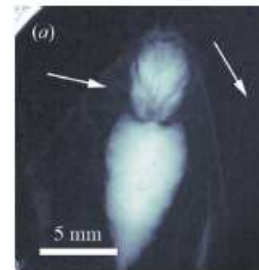
2. Using the central part of the beam

- Diffraction
 - Spectroscopy (fluo, XANES)
 - Radiotherapy
- MATERIEL SCIENCE
- MRT THERAPY ?
(micro/mini beam radiation)

- **bw 2-3%**
- **Small source size** (to have transverse coherence)

[Synch. Rad. 16, 2009, 43-47]

CS Lyncean Tech. (only CCS in operation in the world)



standard absorption

phase-contrast

13.5 KeV , 3% bw
10⁹ ph/sec
 $\sigma = 165 \mu\text{m}$

Proof of principle



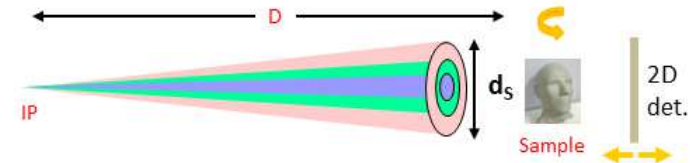
- **70 KeV, 2-3% bw, $\sigma \sim 70 \mu\text{m}$**
- **$d_s = 4 \text{ cm}$ at $D \sim 15 \text{ m}$**
- **10¹² ph/s**

Hospital sources :
large focal spot size, broad spectrum, low flux)

1. Using the 2D divergent beam

- Conventional radiography
 - K-edge subtraction imaging
 - Phase contrast imaging
- IMAGING

- **Radiotherapy**
- THERAPY



- **High energy** (~ 80KeV)



- 80 KeV ± 10 KeV
- $d_s = 5 \text{ cm}$ at $D \sim 10 \text{ m}$
- $3 \cdot 10^{12} \text{ ph/s}$

Ex. : Human head tumor irradiation
(tumor deliver dose ~ 10-20 Gy)

- ThomX → 9 mGy/sec → 20-30 min of irradiation
- ESRF/ID17 (~ 6 mGy/sec)

2. Using the central part of the beam

- Diffraction
 - Spectroscopy (fluo, XANES)
- MATERIEL SCIENCE

- Radiotherapy
- MRT THERAPY ?
(micro/mini beam radiation)



- 80 KeV ± 0.5 KeV
- $d_s = 1 \text{ cm}$ at $D \sim 10 \text{ m}$
- $6 \cdot 10^{10} \text{ ph/s}$

Researches on Photon Activation Therapy

1. Using the 2D divergent beam

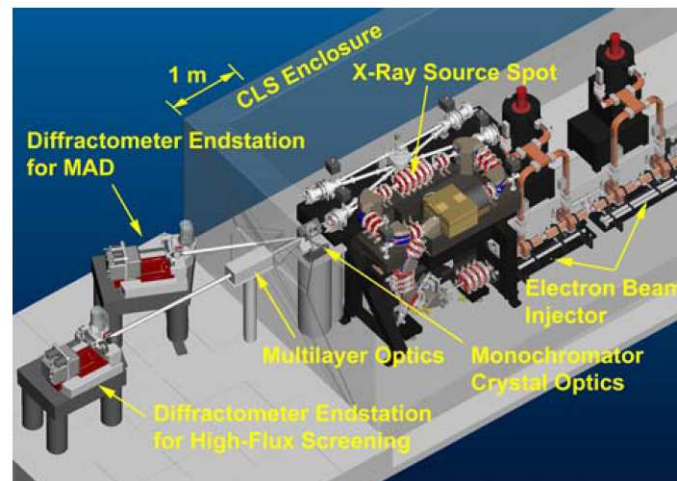
- Conventional radiography
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- IMAGING
- Radiotherapy
- THERAPY

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- MATERIEL SCIENCE
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- MRT THERAPY ?
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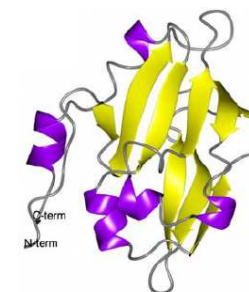
Quasi-monochromatic beam

1st determination of the 3D structure of a protein
CS Lyncean Tech. source



15 KeV, 1.4% bw
5.10⁶ ph/sec
 $\sigma = 120 \mu\text{m}$

Ribbon representation



[J. Struct. Funct. Gen. 11, 2010, 91-100]

Proof of principle (~ Rigaku rotating anode)



• **10⁹ ph/s** , $\Delta E/E \sim 10^{-2} - 10^{-3}$



1. Using the 2D divergent beam

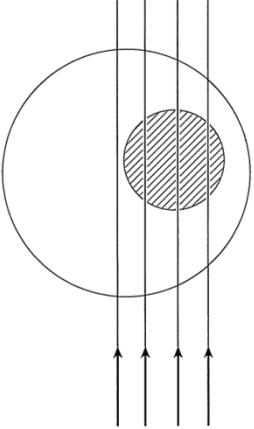
- Conventional radiography
 - K-edge subtraction imaging
 - Phase contrast imaging
-) IMAGING
- Radiotherapy
-) THERAPY

2. Using the central part of the beam

- Diffraction
 - Spectroscopy (fluor, XANES)
-) MATERIEL SCIENCE
- **Radiotherapy**
- MRT THERAPY ?** →
(micro/mini beam radiation)

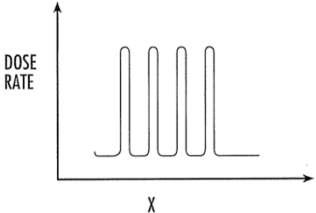
MRT R&D ?

Microbeam Radiotherapy (MRT)
Ability to **eradicate tumors** while **sparing normal tissue**

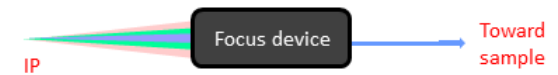


Typically :

MRT uses arrays of narrow **25-75 μm wide microbeams** separated by **100-400 μm spaces**.



(Feasibility studies started in the SYRA3 working group)



- **CCS combine**

- Compactness
- High flux/brightness
- Tunable energy
- Transverse coherence

- **The machines of today**

- Hot machines
- Flux $\sim 10^{13}$
- Brightness $\sim 10^{11}$

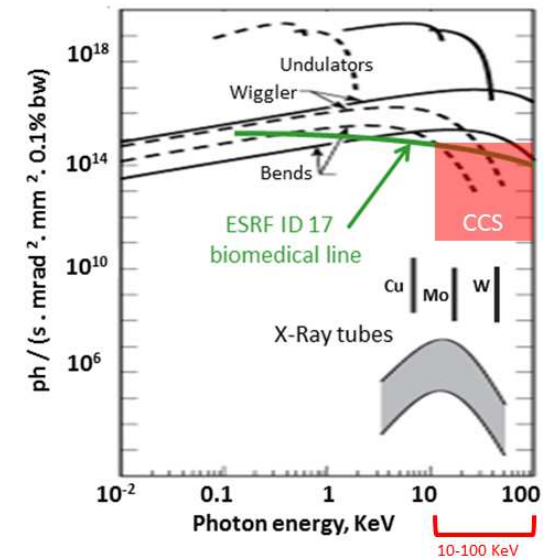


- **... and tomorrow**

- Supra machines (e- gun)
- Flux $\sim 10^{13}$ - 10^{14}
- Brightness $\sim 10^{13}$ - 10^{15}

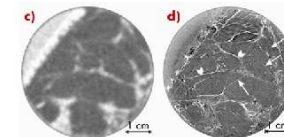
Two strong challenges remain

- Superconducting injector (100 MHz, very small emittance)
- Radioprotection shielding for integration



- → **Fill the great lack of intense and bright lab sources**

Develop in lab size environments powerful analysis techniques currently used only at synchrotrons.



1. With the large 2D Compton beam

$\sim 10^{12}$ - 10^{13} ph/s , 10% bw , few centimeters beam

- Conventional imaging
 - K-edge
 - Phase contrast
 - Radiotherapy
 - High-Z drug tests
- with the great advantage of a large 2D beam (compared to synchrotrons)

2. With the focus central part of the beam

$\sim 10^9$ ph/s , 0.1-1% bw , mm beam

- Diffraction
- Spectroscopy
- MRT ?