

# DEVELOPMENT OF NEW DOSIMETRIC STANDARDS FOR LOW ENERGY X-RAYS ( $\leq 50$ keV) USED IN RADIOTHERAPY

PHENIICS Days, 9-11 May 2016 | Abdullah ABUDRA'A

**list**



**LNHB**



Laboratoire National Henri Becquerel

## CONTACT RADIOTHERAPY

## CONTACT RADIOTHERAPY

- Radiation source is in contact with the tumor cells.

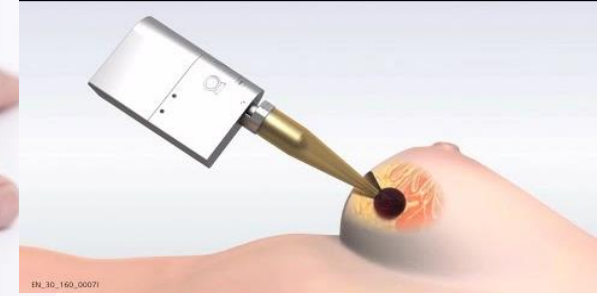
## CONTACT RADIOTHERAPY

- Radiation source is in contact with the tumor cells.



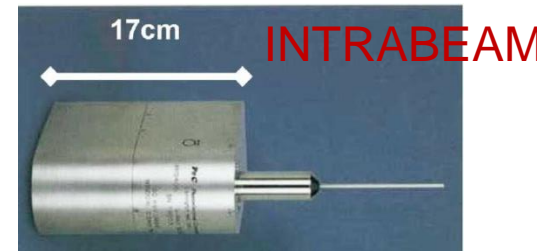
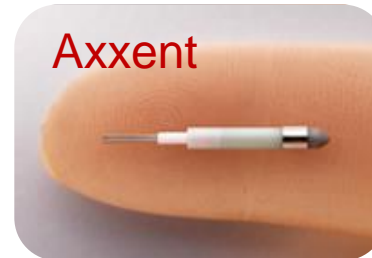
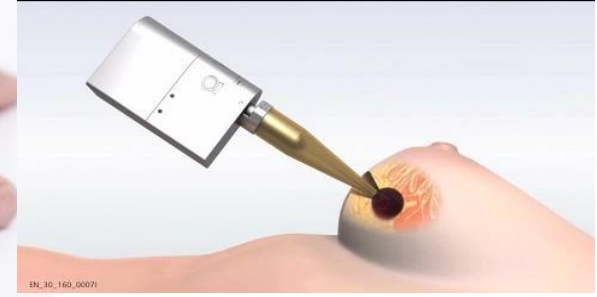
## CONTACT RADIOTHERAPY

- Radiation source is in contact with the tumor cells.



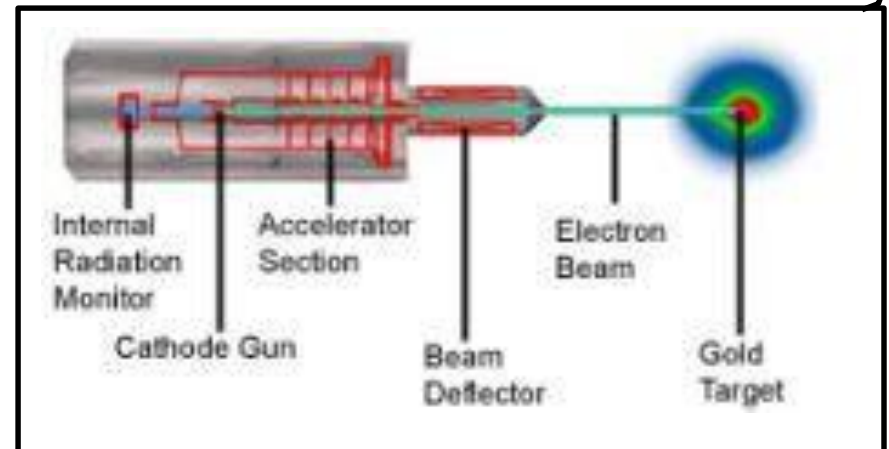
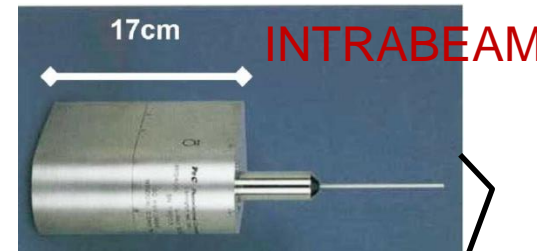
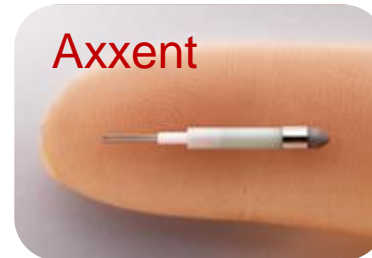
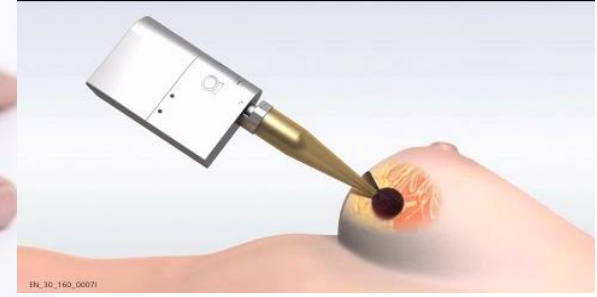
## CONTACT RADIOTHERAPY

- Radiation source is in contact with the tumor cells.



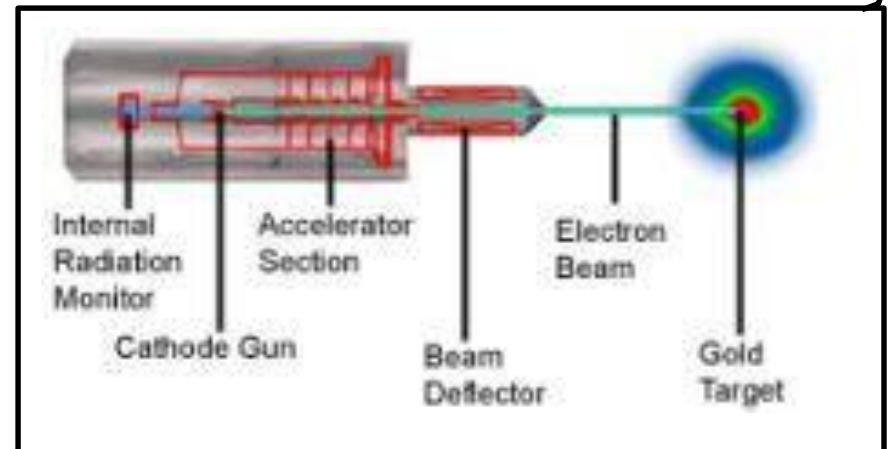
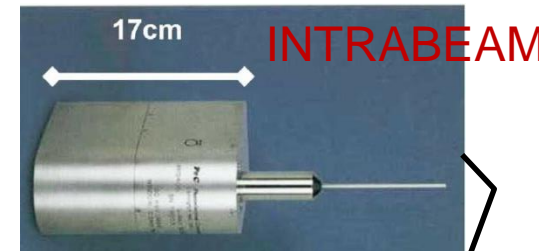
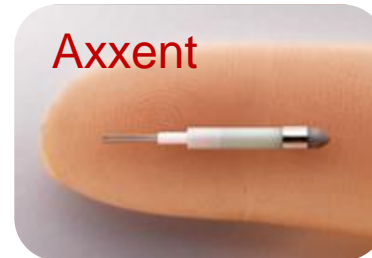
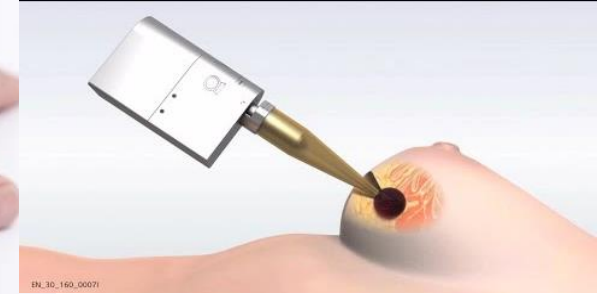
## CONTACT RADIOTHERAPY

- Radiation source is in contact with the tumor cells.



## CONTACT RADIOTHERAPY

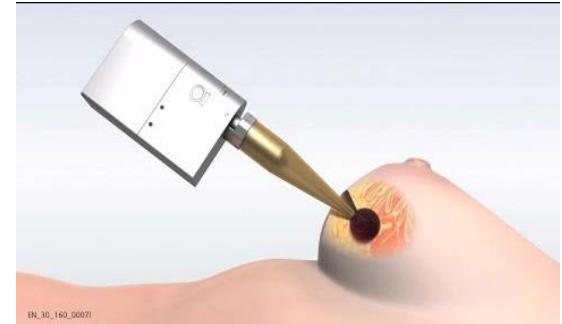
- Radiation source is in contact with the tumor cells.
- Characteristics:
  - Low penetration → Low energy X-rays  $\leq 50$  keV
  - More preservation (protection) for healthy tissues
  - Higher dose can be delivered → Lower treatment time ( more comfort and lower cost)





## THE INTRABEAM SYSTEM

- Widely used in France for breast cancer.



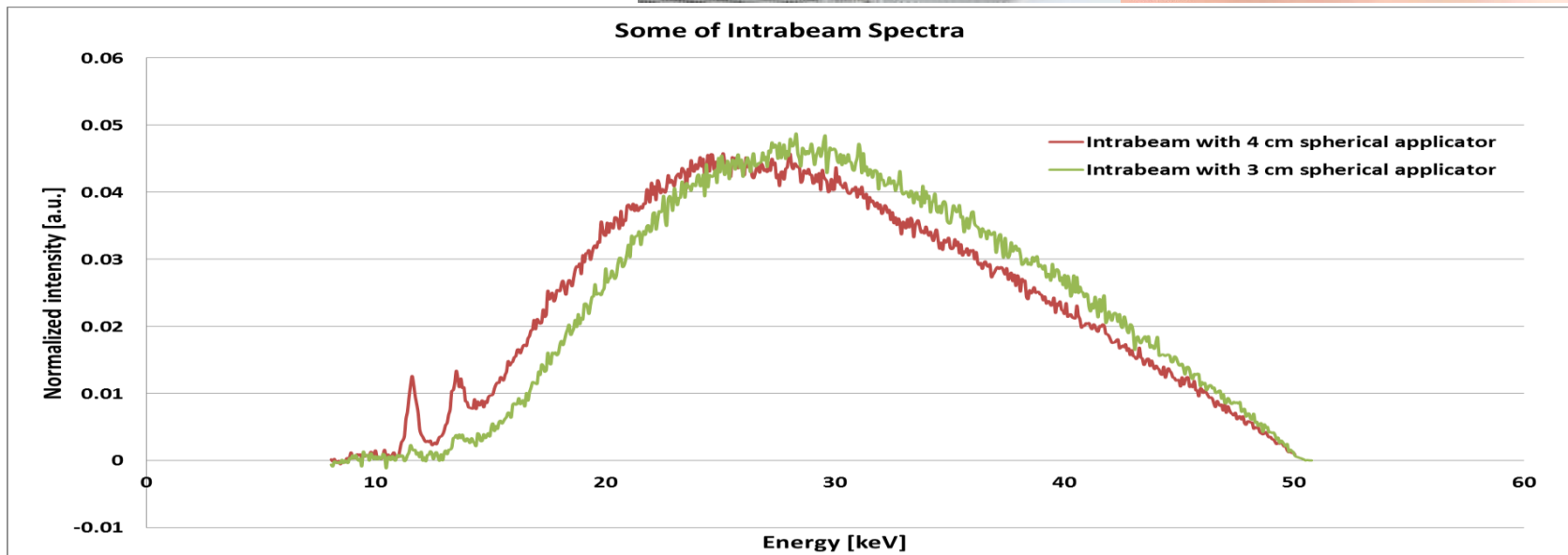
## THE INTRABEAM SYSTEM

- Widely used in France for breast cancer.
- Variety of applicators to adapt with cancer size.



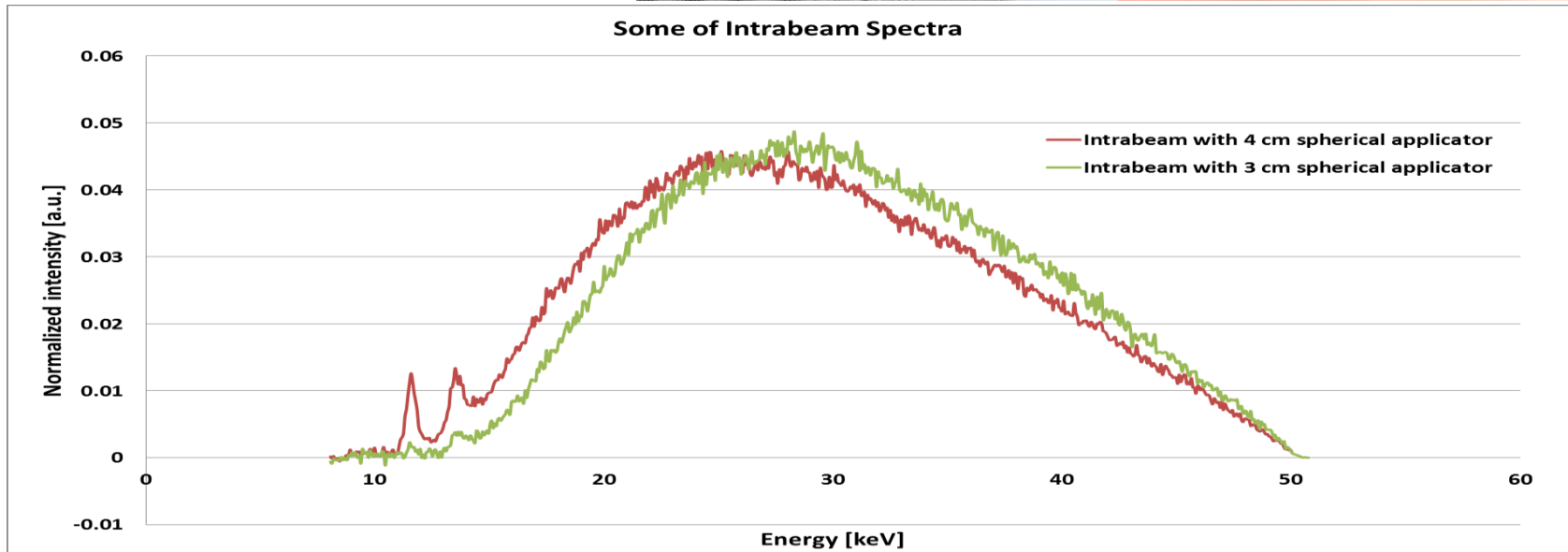
## THE INTRABEAM SYSTEM

- Widely used in France for breast cancer.
- Variety of applicators to adapt with cancer size.



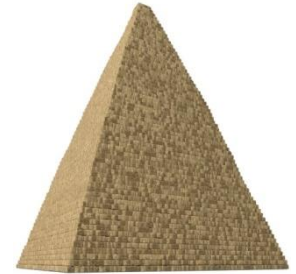
## THE INTRABEAM SYSTEM

- Widely used in France for breast cancer.
- Variety of applicators to adapt with cancer size.

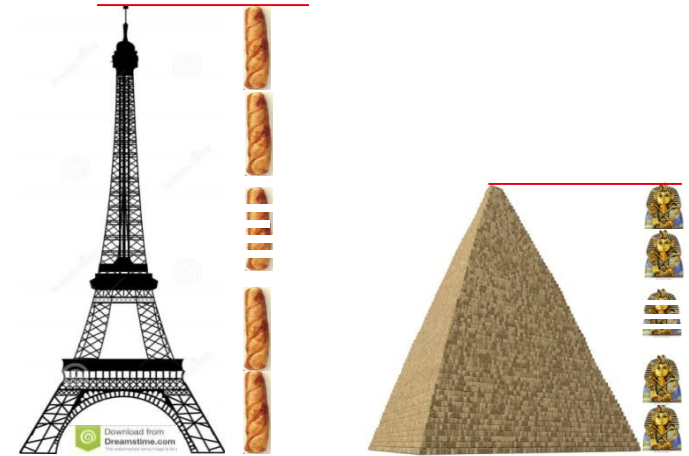


- Only dose distribution data of the manufacturer! → Need for a dosimetric standard!

Which is higher?



Which is higher?



Which is higher?

We need then:

- To agree on a unit, Quantity ...
- A device, system, tool ... →  
Measure

A **Standard**



## Quantities defined for dose measurements (at a Point):

- Absorbed dose to water,  $D_w$
- Air kerma,  $K_{air}$



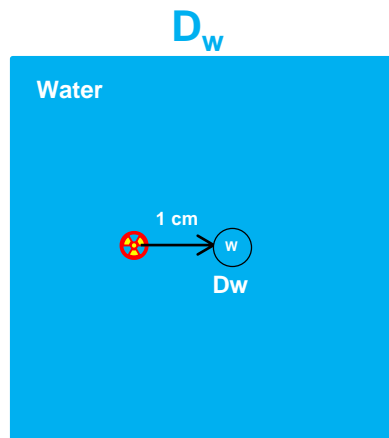
## Quantities defined for dose measurements (at a Point):

- Absorbed dose to water,  $D_w$
- Air kerma,  $K_{air}$

- $D_w$ : Energy Deposited per unit mass

$$\frac{\text{Energy}}{\text{Mass}} \rightarrow \text{J. Kg}^{-1} = \text{Gy}$$

Standard configurations:



## Quantities defined for dose measurements (at a Point):

- Absorbed dose to water,  $D_w$
- Air kerma,  $K_{air}$

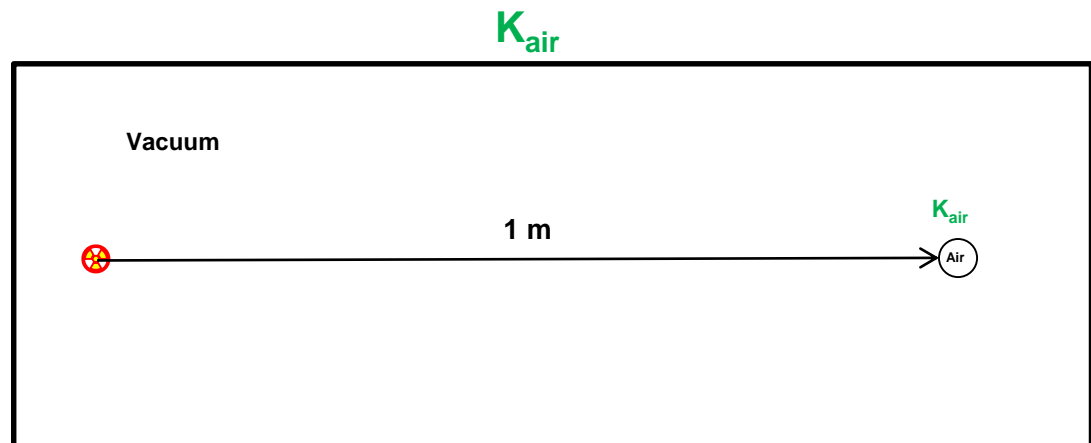
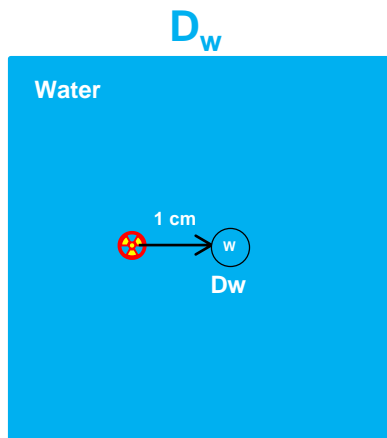
•  $D_w$  : Energy Deposited per unit mass

•  $K_{air}$  : Energy Transferred per unit mass

$$\frac{Energy}{Mass} \rightarrow J. Kg^{-1} = Gy$$

$$\frac{Energy}{Mass} \rightarrow J. Kg^{-1} = Gy$$

Standard configurations:



## PROCEDURE TO ESTABLISH THE DOSIMETRIC STANDARD

- The dosimetric standard is established at Henri Becquerel National Laboratory (LNHB)

## PROCEDURE TO ESTABLISH THE DOSIMETRIC STANDARD

- **The dosimetric standard is established at Henri Becquerel National Laboratory (LNHB)**
  - French Primary standard laboratory for ionizing radiation.
  - provides the dosimetric quantities with the highest accuracy (lowest) uncertainty.

## PROCEDURE TO ESTABLISH THE DOSIMETRIC STANDARD

- **The dosimetric standard is established at Henri Becquerel National Laboratory (LNHB)**
  - French Primary standard laboratory for ionizing radiation.
  - provides the dosimetric quantities with the highest accuracy (lowest) uncertainty.
- **Steps of calibration procedure, in terms of  $K_{\text{air}}$ :**

## PROCEDURE TO ESTABLISH THE DOSIMETRIC STANDARD

- **The dosimetric standard is established at Henri Becquerel National Laboratory (LNHB)**
  - French Primary standard laboratory for ionizing radiation.
  - provides the dosimetric quantities with the highest accuracy (lowest) uncertainty.
- **Steps of calibration procedure, in terms of  $K_{\text{air}}$ :**
  1. Reproduction of spectra
  2. Establishment of the air kerma standard
  3. Calibration of secondary transfer ionization chambers

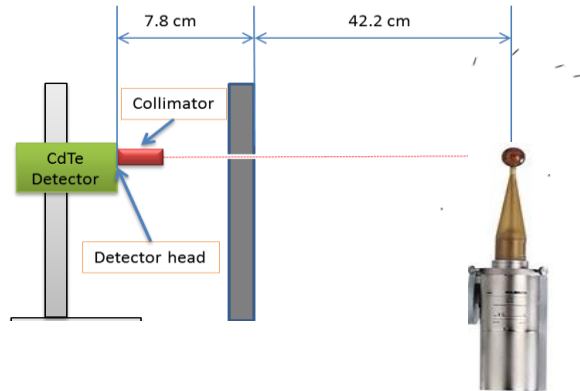
## PROCEDURE TO ESTABLISH THE DOSIMETRIC STANDARD

- **The dosimetric standard is established at Henri Becquerel National Laboratory (LNHB)**
  - French Primary standard laboratory for ionizing radiation.
  - provides the dosimetric quantities with the highest accuracy (lowest) uncertainty.
- **Steps of calibration procedure, in terms of  $K_{\text{air}}$ :**
  1. Reproduction of spectra
  2. Establishment of the air kerma standard
  3. Calibration of secondary transfer ionization chambers



Using the  $K_{\text{air}}$  standard and the calibrated IC to measure the depth dose profile

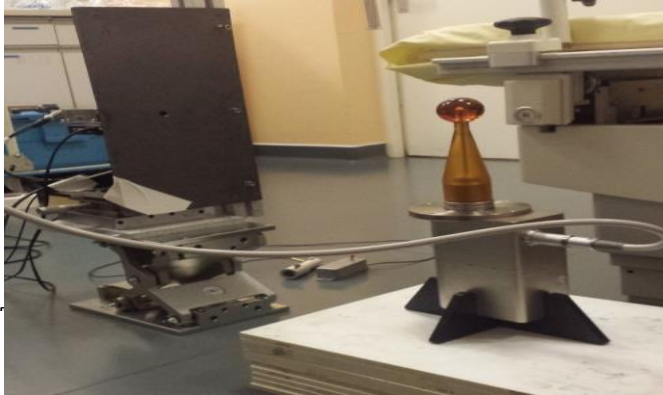
## REPRODUCTION OF INTRABEAM SPECTRA



Measurement of INTRABEAM spectra at  
Saint Louis Hospital in Paris

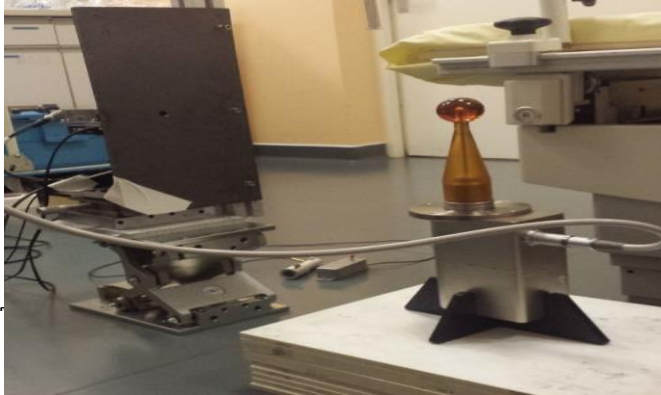


## REPRODUCTION OF INTRABEAM SPECTRA

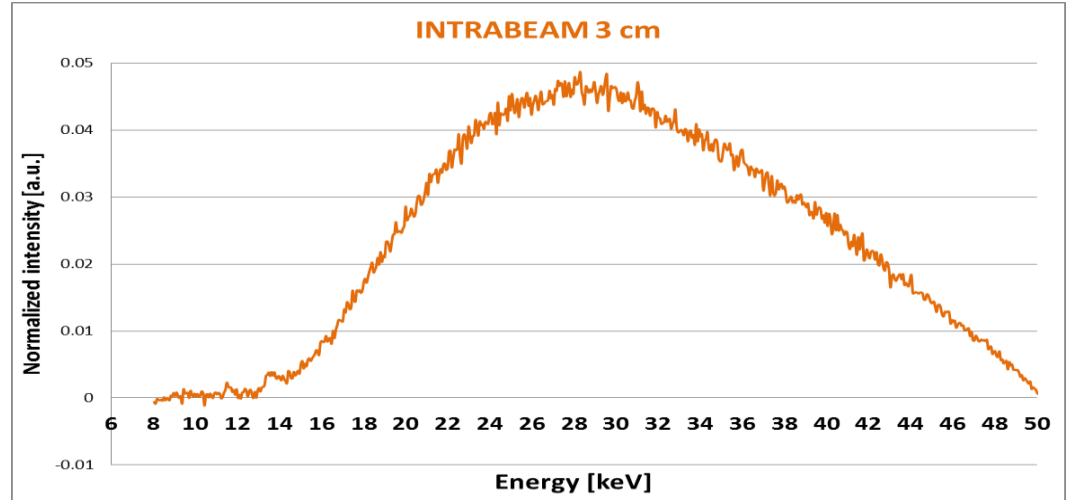


Measurement of INTRABEAM spectra at Saint Louis Hospital in Paris

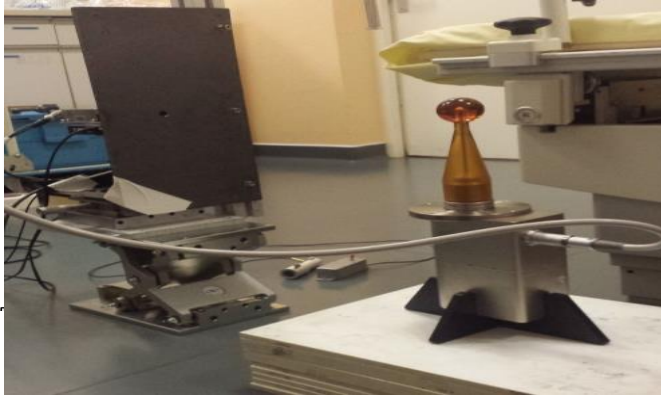
## REPRODUCTION OF INTRABEAM SPECTRA



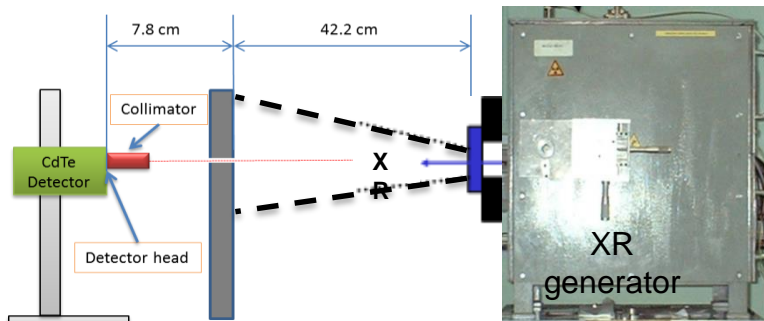
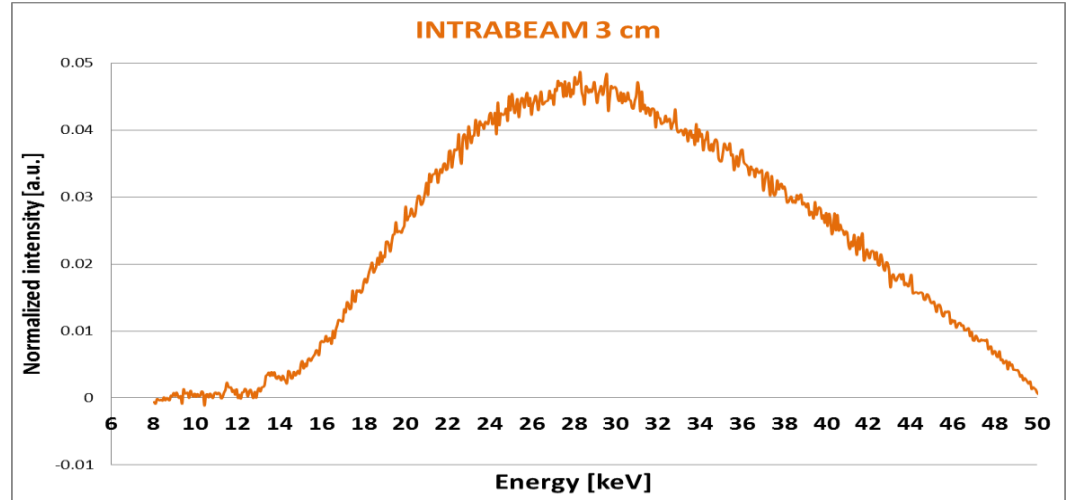
Measurement of INTRABEAM spectra at Saint Louis Hospital in Paris



## REPRODUCTION OF INTRABEAM SPECTRA

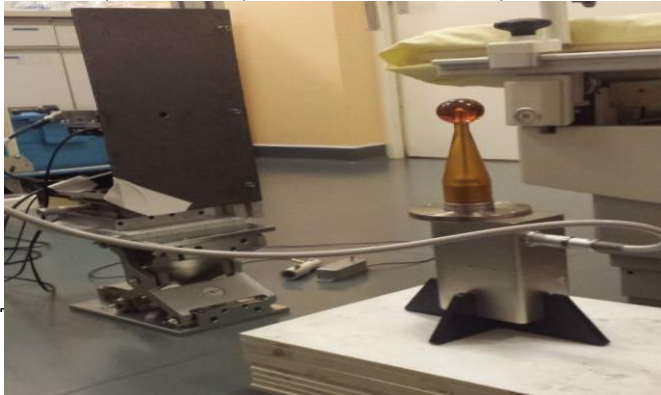


Measurement of INTRABEAM spectra at Saint Louis Hospital in Paris

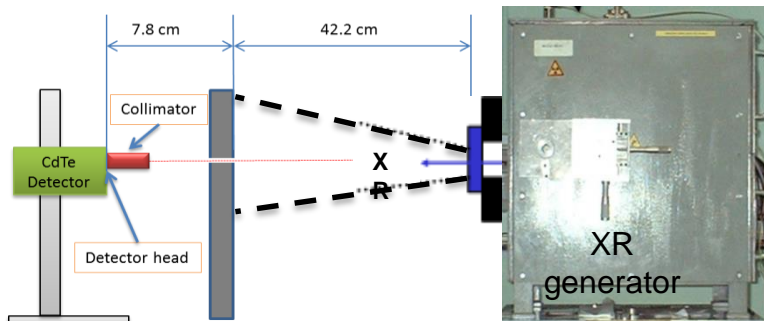
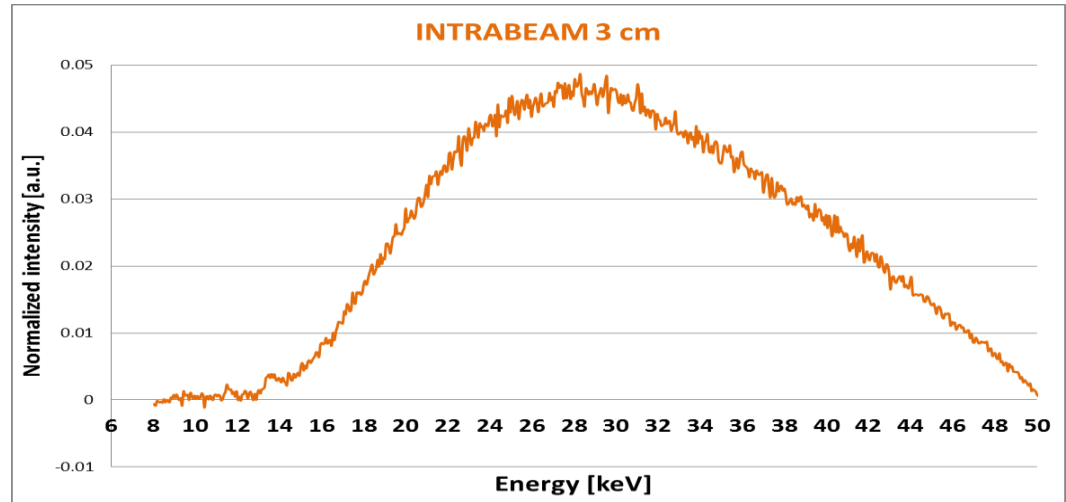


Reproduction of INTRABEAM spectra with the XR generator with 1.75 mm Al filter

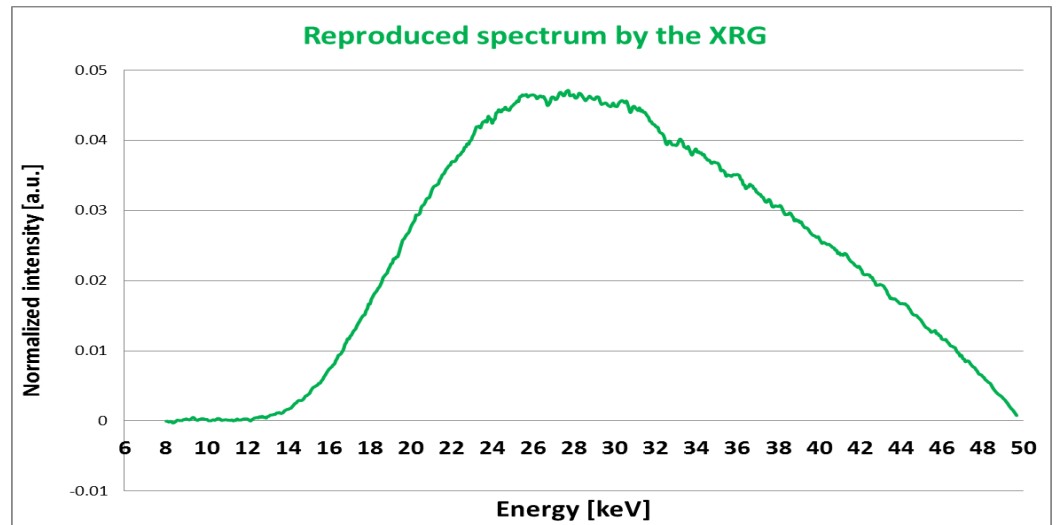
## REPRODUCTION OF INTRABEAM SPECTRA



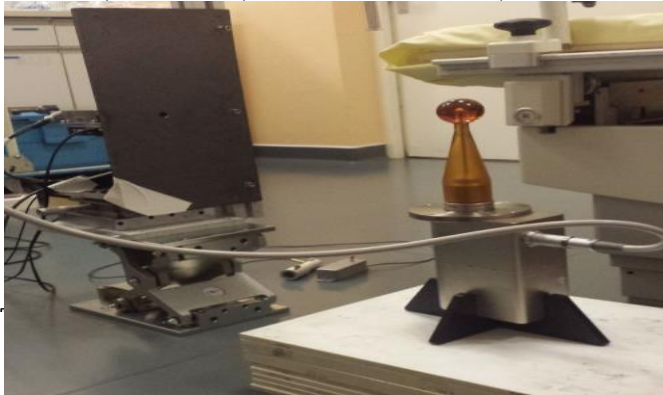
Measurement of INTRABEAM spectra at Saint Louis Hospital in Paris



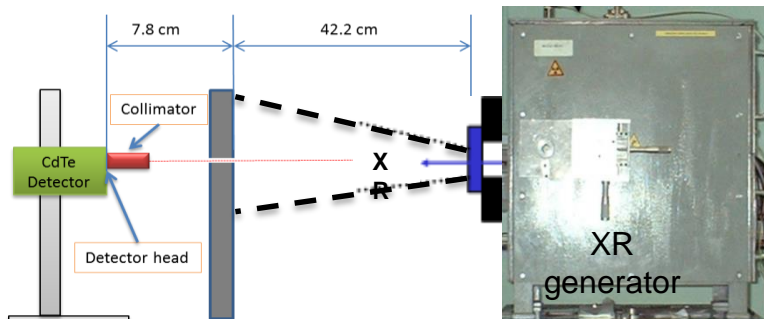
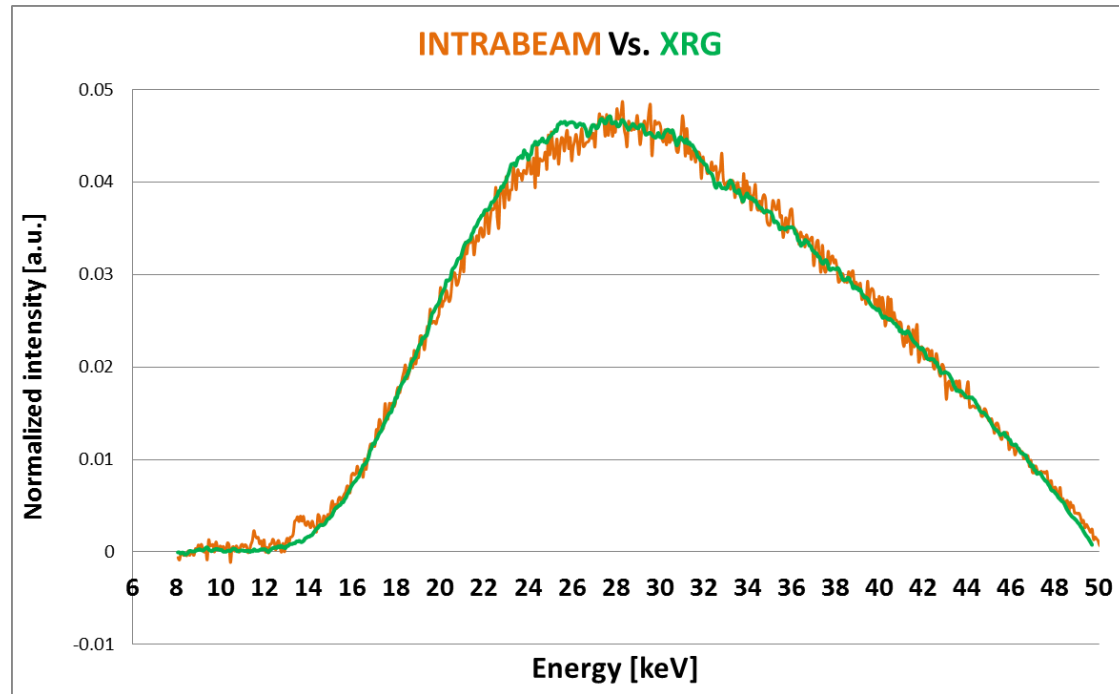
Reproduction of INTRABEAM spectra with the XR generator with 1.75 mm Al filter



## REPRODUCTION OF INTRABEAM SPECTRA



Measurement of INTRABEAM spectra at Saint Louis Hospital in Paris



Reproduction of INTRABEAM spectra with the XR generator with 1.75 mm Al filter

## VALIDATION OF REPRODUCED SPECTRA

## VALIDATION OF REPRODUCED SPECTRA

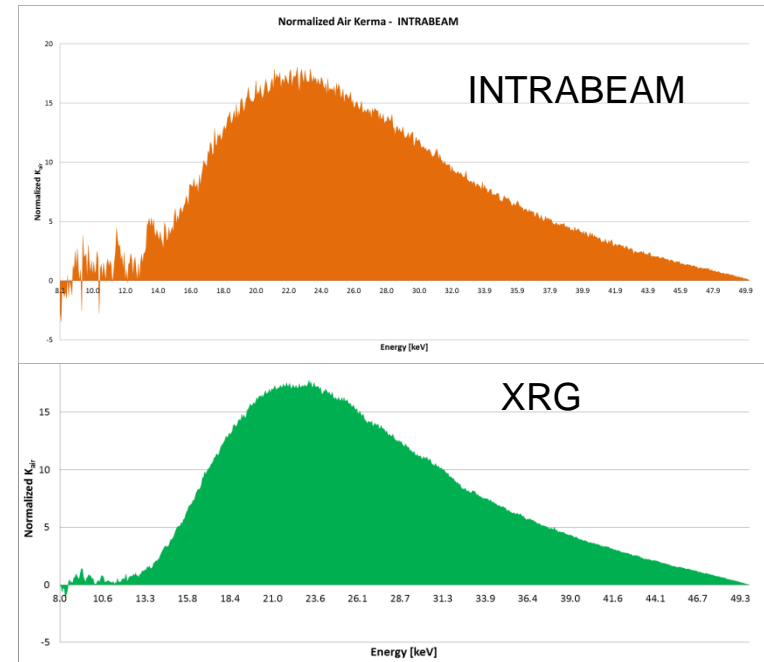
$$K_{\text{air,norm}} = \sum \left[ \frac{\phi(E)}{[\sum \phi(E) \Delta E]} \cdot \left( \frac{\mu_{tr}(E)}{\rho} \right)_{\text{air}} \cdot E \cdot \Delta E \right]$$

Normalized air kerma,  $K_{\text{air,norm}}$  → To validate the agreement between the two spectra by quantifying the total normalized air kerma of each spectrum.

## VALIDATION OF REPRODUCED SPECTRA

$$K_{\text{air,norm}} = \sum \left[ \frac{\phi(E)}{[\sum \phi(E) \Delta E]} \cdot \left( \frac{\mu_{tr}(E)}{\rho} \right)_{\text{air}} \cdot E \cdot \Delta E \right]$$

Normalized air kerma,  $K_{\text{air,norm}}$  → To validate the agreement between the two spectra by quantifying the total normalized air kerma of each spectrum.

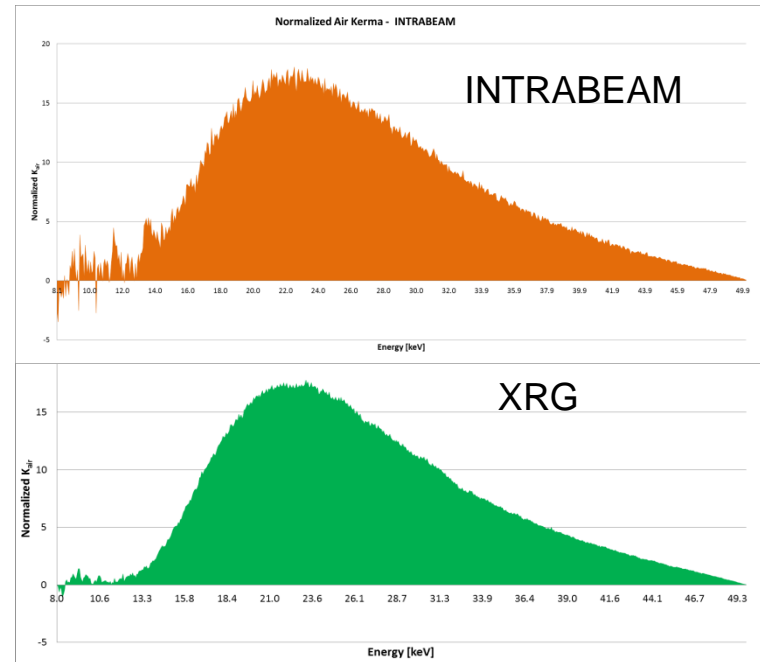




## VALIDATION OF REPRODUCED SPECTRA

$$K_{air,norm} = \sum \left[ \frac{\phi(E)}{[\sum \phi(E) \Delta E]} \cdot \left( \frac{\mu_{tr}(E)}{\rho} \right)_{air} \cdot E \cdot \Delta E \right]$$

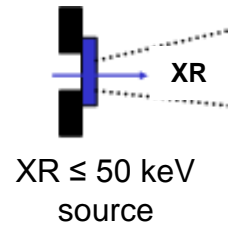
Normalized air kerma,  $K_{air,norm}$  → To validate the agreement between the two spectra by quantifying the total normalized air kerma of each spectrum.



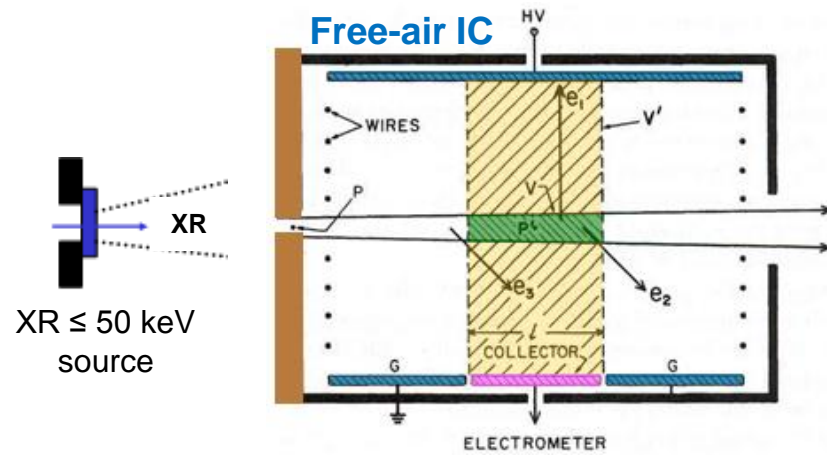
3 cm spherical applicator	
$\frac{K_{air,norm}(XRG)}{K_{air,norm}(INTRABEAM)}$	<h1>0.40 %</h1>

## Establishment of the $\dot{K}_{air}$ standard

## Establishment of the $\dot{K}_{air}$ standard

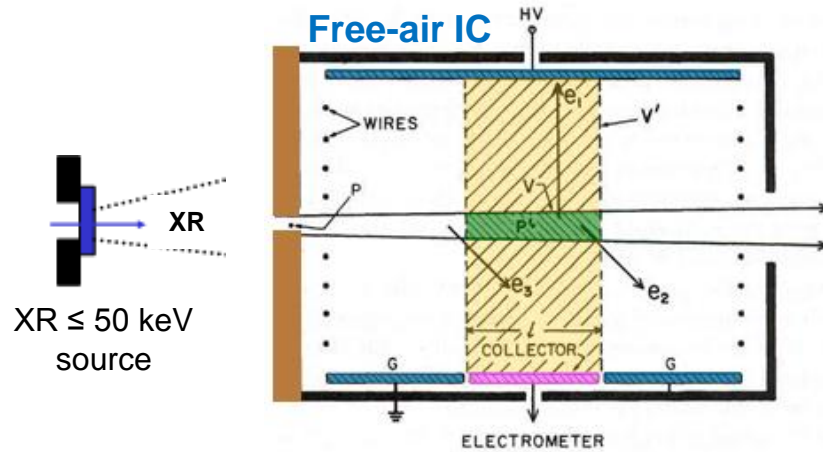


## Establishment of the $K_{air}$ standard



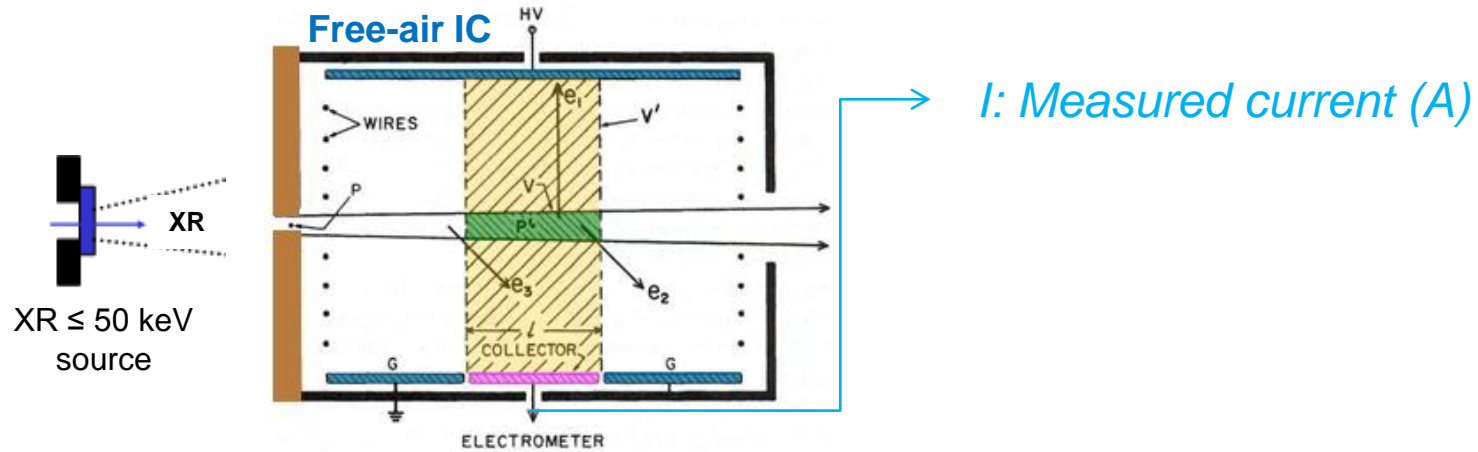
## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



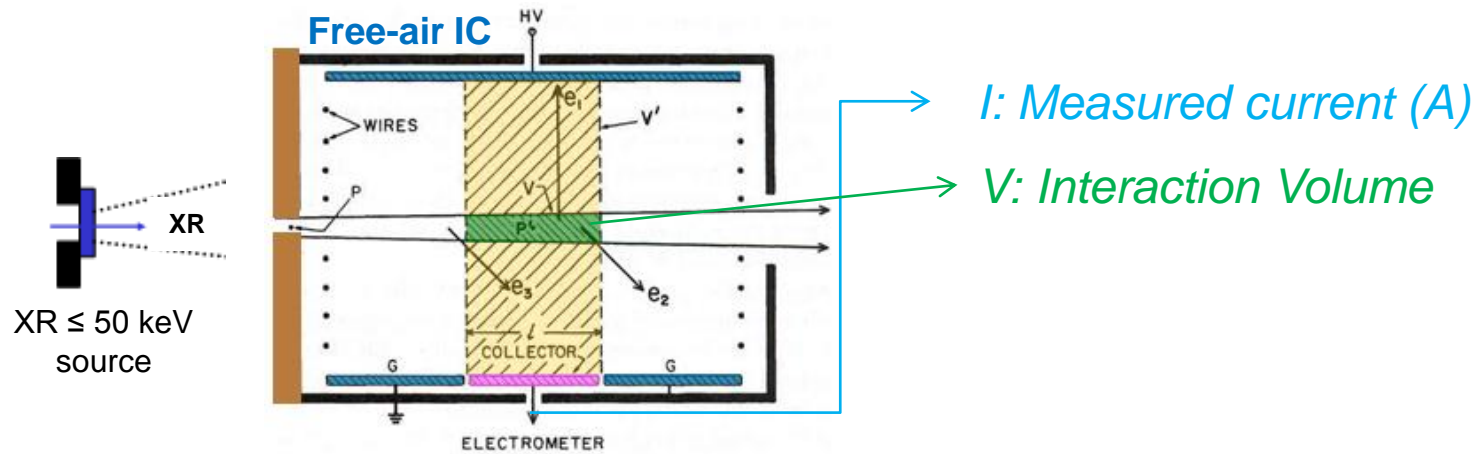
## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



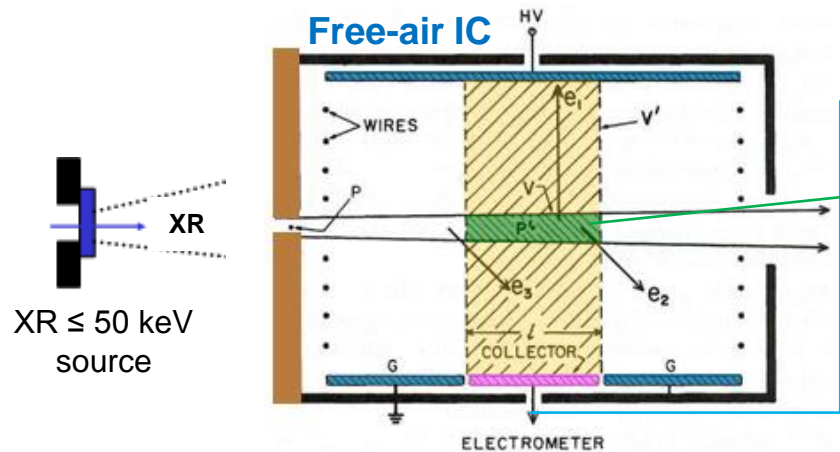
## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



$I$ : Measured current (A)

$V$ : Interaction Volume

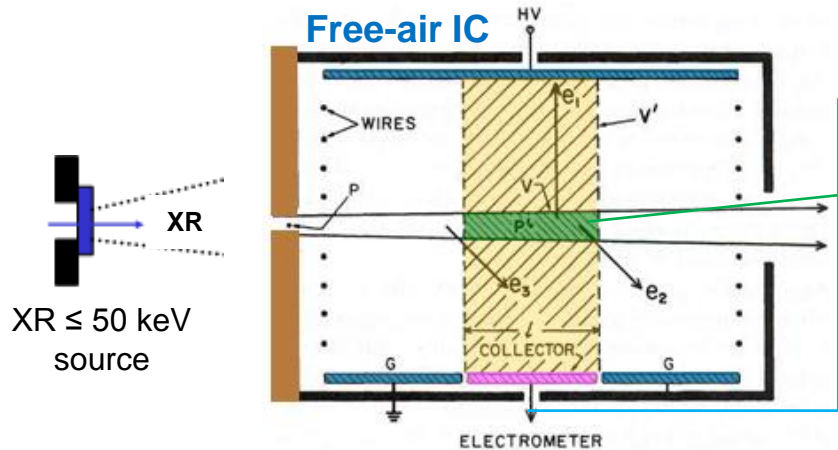
Physical parameters:

$\rho_0$ ; Air density,  $\frac{W_{air}}{e}$ ; Avg. Energ. Of ion-pair creation, ...



## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



$I$ : Measured current (A)

$V$ : Interaction Volume

Physical parameters:

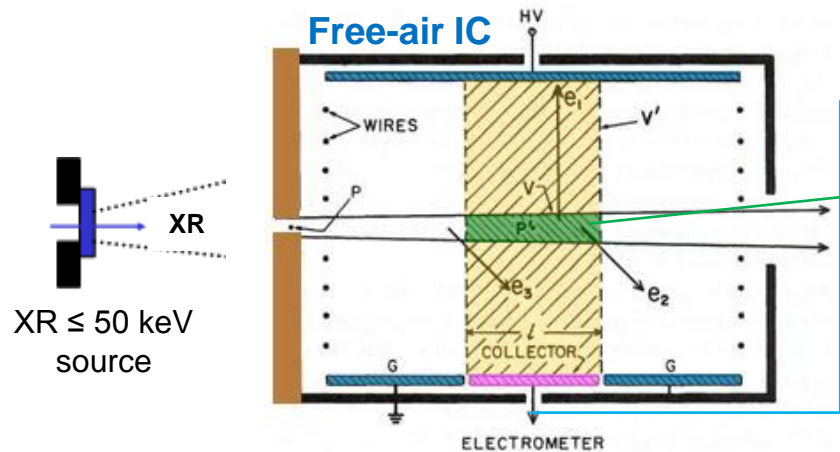
$\rho_0$ ; Air density,  $\frac{W_{air}}{e}$ ; Avg. Energ. Of ion-pair creation, ...

Correction factors

$$\prod_i k_i = k_{sc} \cdot k_a \cdot k_l \cdot k_{pol} \cdot k_s \dots$$

## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



$I$ : Measured current (A)

$V$ : Interaction Volume

Physical parameters:

$\rho_0$ ; Air density,  $\frac{W_{air}}{e}$ ; Avg. Energ. Of ion-pair creation, ...

Correction factors

$$\prod_i k_i = k_{sc} \cdot k_a \cdot k_l \cdot k_{pol} \cdot k_s \dots$$

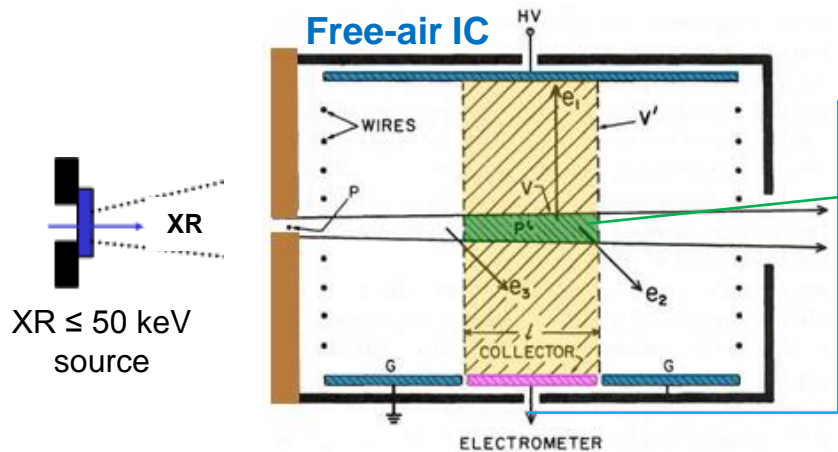
$k_{sc}$ : Scattered radiation

$k_a$ : Air attenuation

$k_l$ : Aperture transmission

## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



$I$ : Measured current (A)

$V$ : Interaction Volume

Physical parameters:

$\rho_0$ ; Air density,  $\frac{W_{air}}{e}$ ; Avg. Energ. Of ion-pair creation, ...

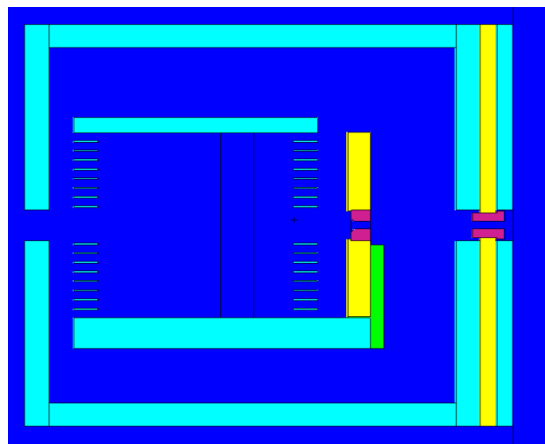
Correction factors

$$\prod_i k_i = k_{sc} \cdot k_a \cdot k_l \cdot k_{pol} \cdot k_s \dots$$

$k_{sc}$ : Scattered radiation

$k_a$ : Air attenuation

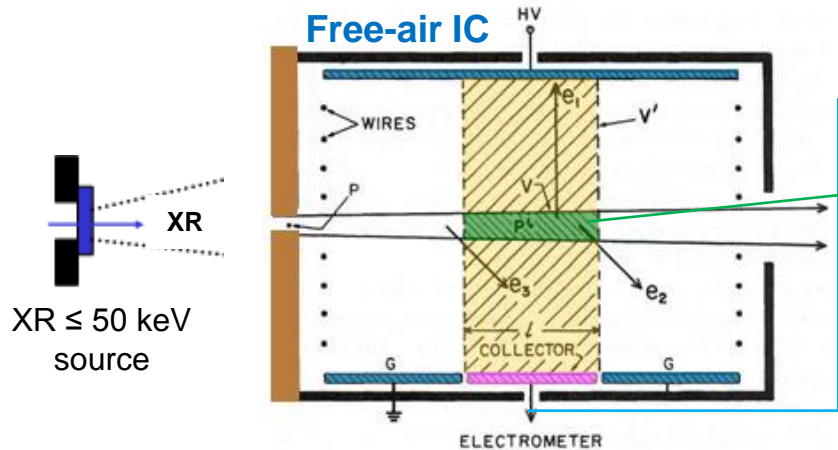
$k_l$ : Aperture transmission



Monte carlo simulation

## Establishment of the $\dot{K}_{air}$ standard

$$\dot{K}_{air} = \frac{I}{V \cdot \rho_0} \cdot \frac{W_{air}}{e} \cdot \frac{1}{(1 - g_{air})} \cdot \prod_i k_i$$



$I$ : Measured current (A)

$V$ : Interaction Volume

Physical parameters:

$\rho_0$ ; Air density,  $\frac{W_{air}}{e}$ ; Avg. Energ. Of ion-pair creation, ...

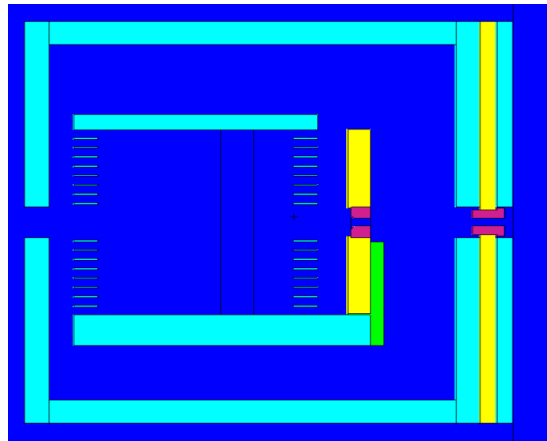
Correction factors

$$\prod_i k_i = k_{sc} \cdot k_a \cdot k_l \cdot k_{pol} \cdot k_s \dots$$

$k_{sc}$ : Scattered radiation

$k_a$ : Air attenuation

$k_l$ : Aperture transmission



Monte carlo simulation

# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

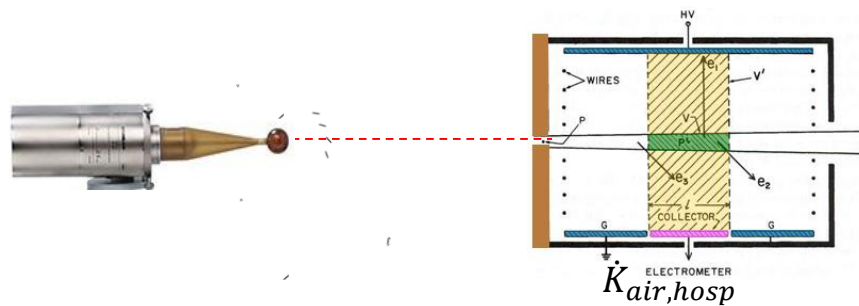
# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In Hospitals



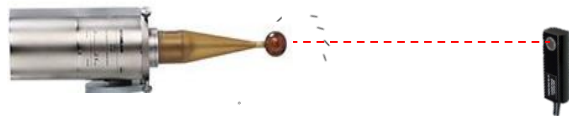
# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In Hospitals



## CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In Hospitals



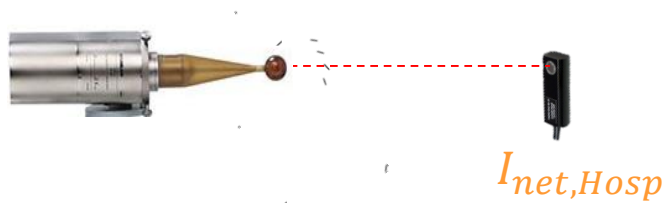
$I_{net,Hosp}$



# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

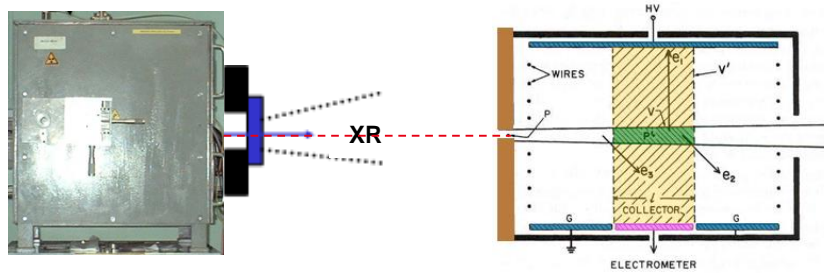
In LNHB Laboratory

In Hospitals

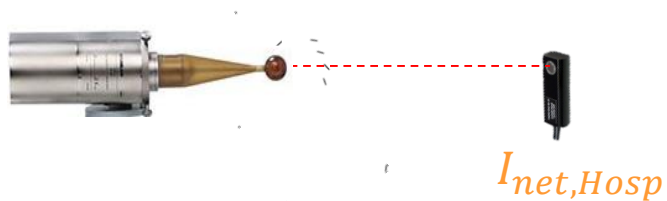


# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In LNHB Laboratory

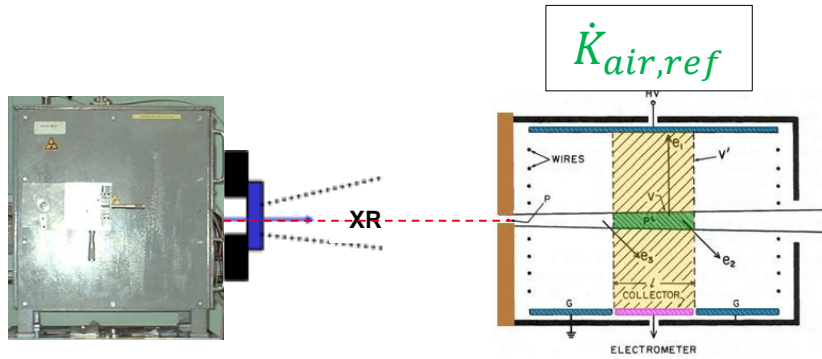


In Hospitals

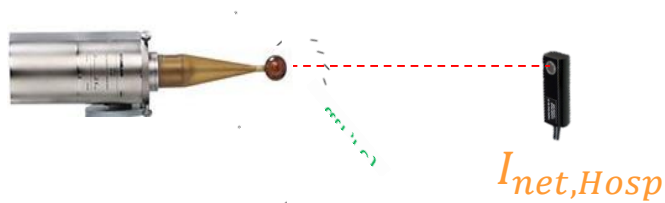


# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In LNHB Laboratory

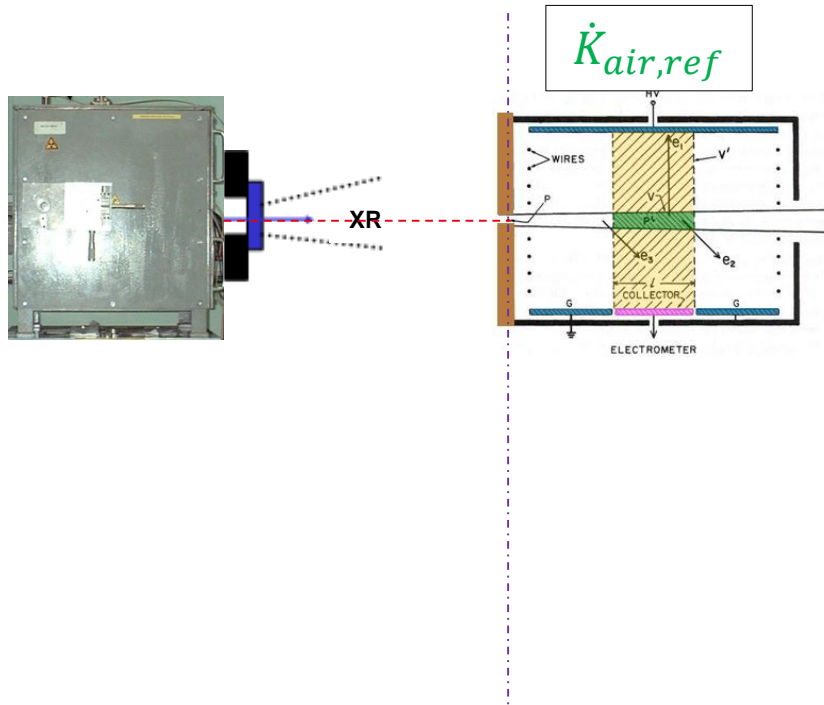


In Hospitals

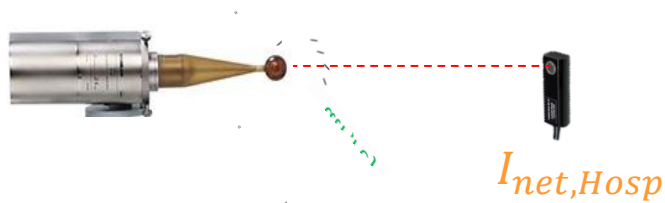


# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In LNHB Laboratory

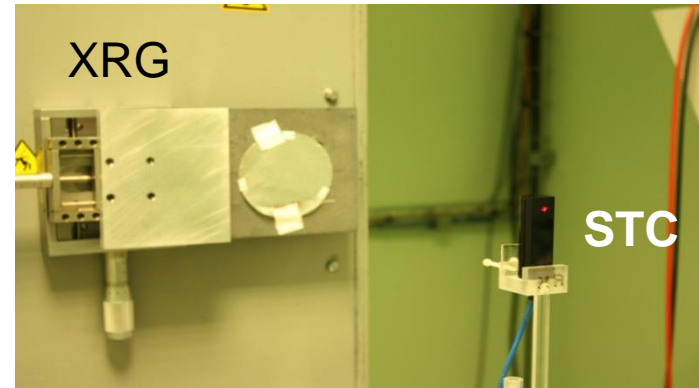
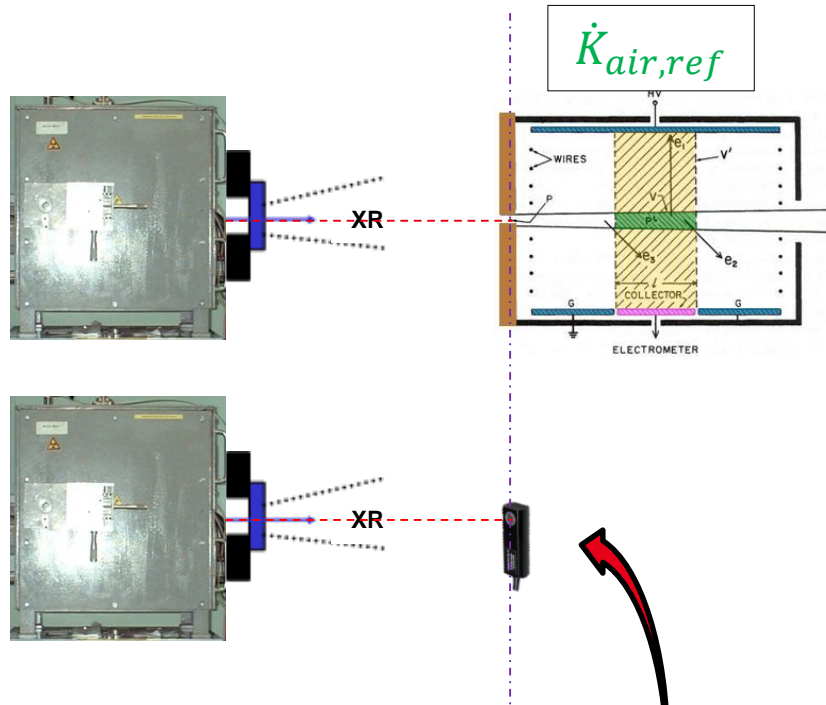


In Hospitals

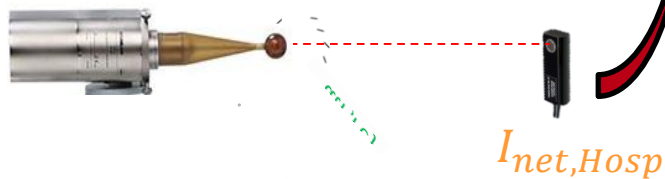


# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In LNHB Laboratory

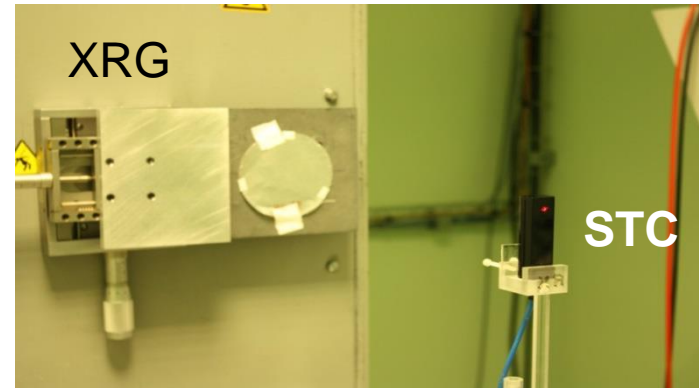
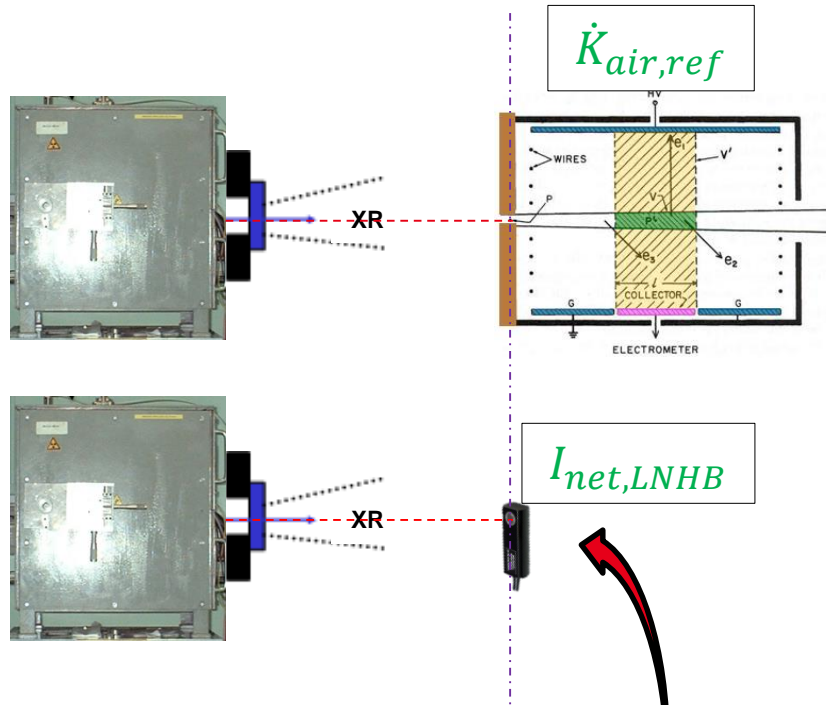


In Hospitals

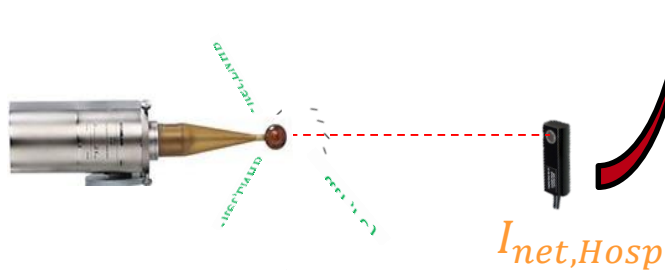


# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In LNHB Laboratory

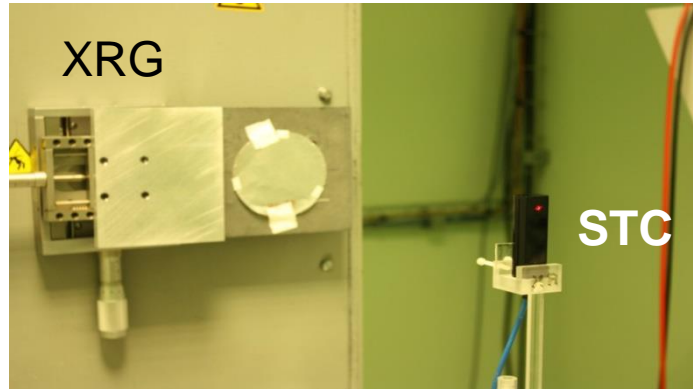
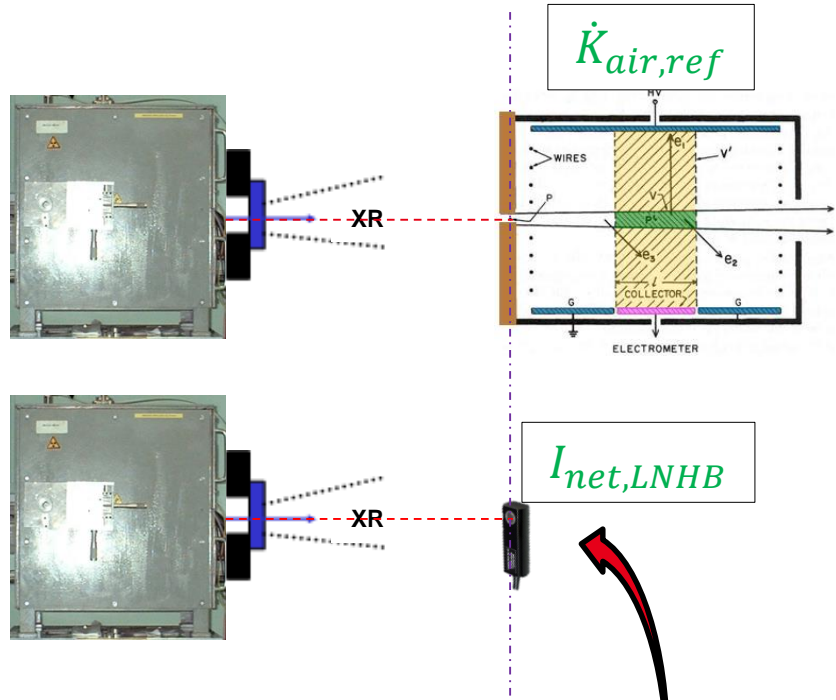


In Hospitals

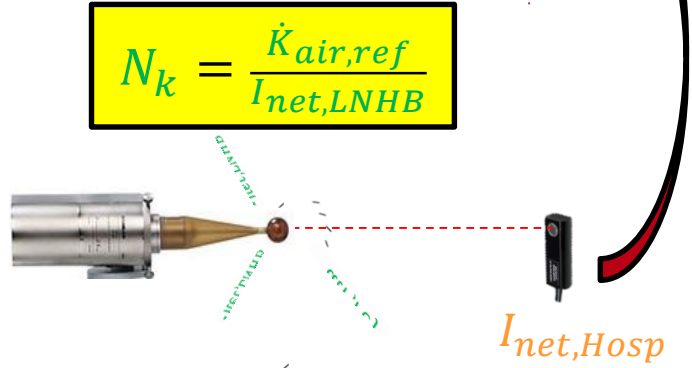


# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In LNHB Laboratory

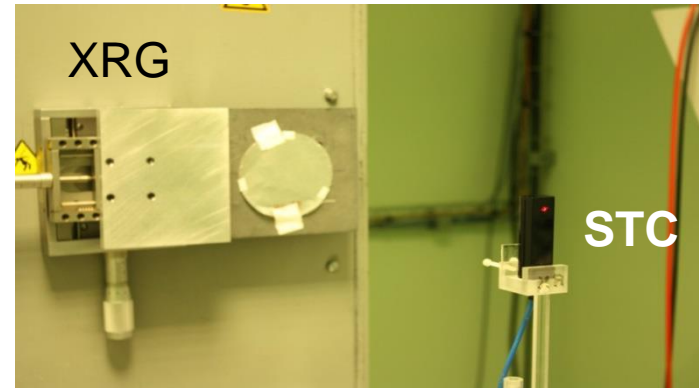
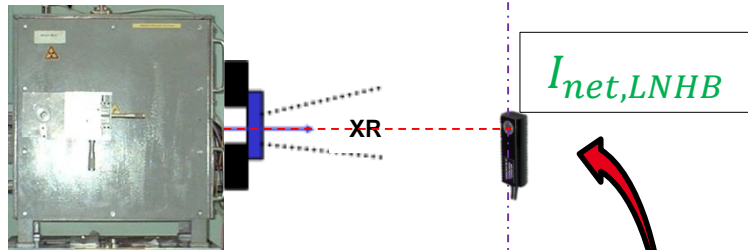
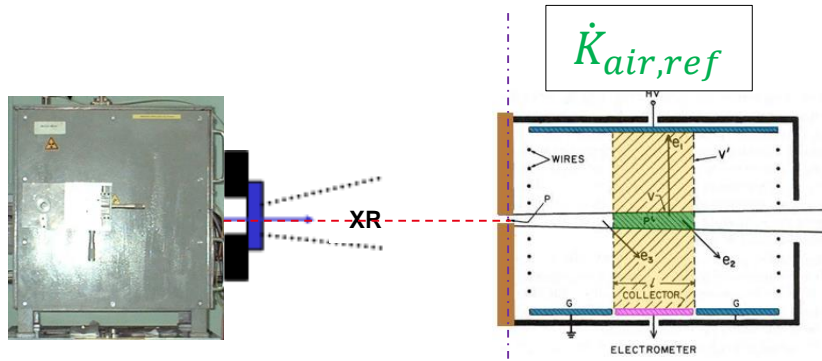


In Hospitals



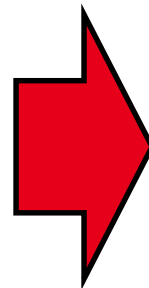
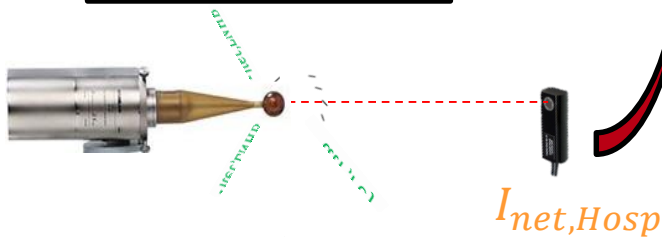
# CALIBRATION OF HOSPITALS/INSTITUTES READING CHAMBERS

In LNHB Laboratory



In Hospitals

$$N_k = \frac{\dot{K}_{air,ref}}{I_{net, LNHB}}$$



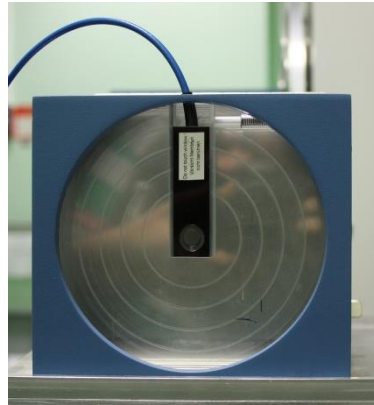
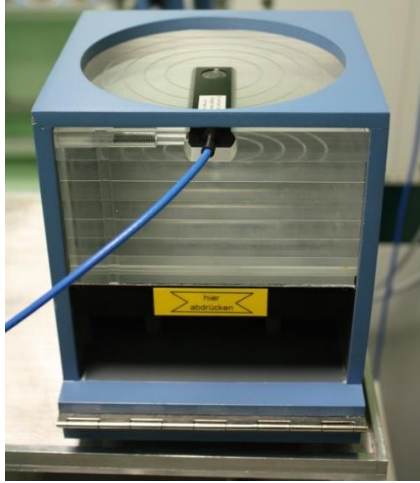
$$\dot{K}_{air,hosp} = I_{net,Hosp} \times N_k$$



## DEPTH DOSE PROFILE DETERMINATION:

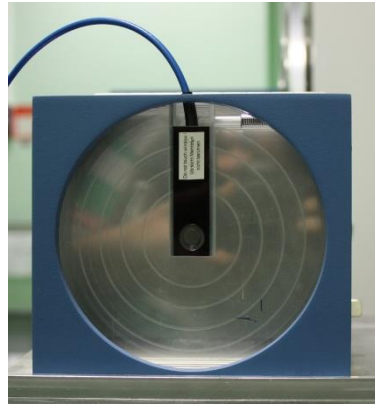
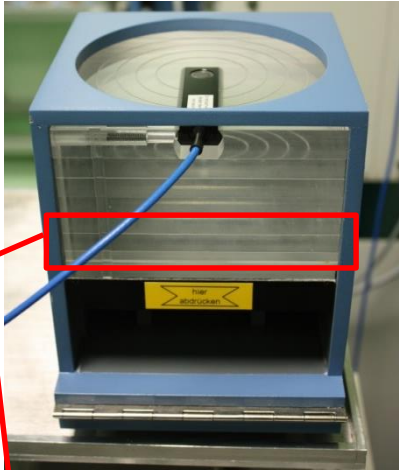
## DEPTH DOSE PROFILE DETERMINATION:

First approach to the  $D_w$



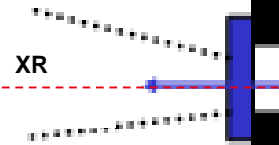
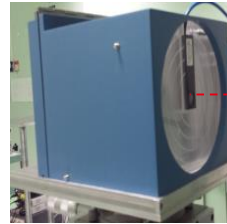
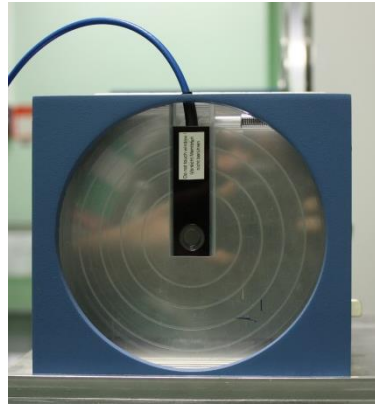
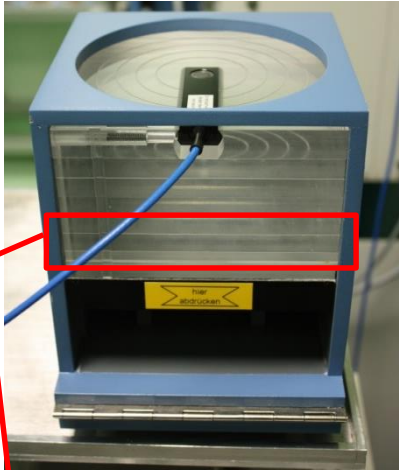
## DEPTH DOSE PROFILE DETERMINATION:

First approach to the  $D_w$



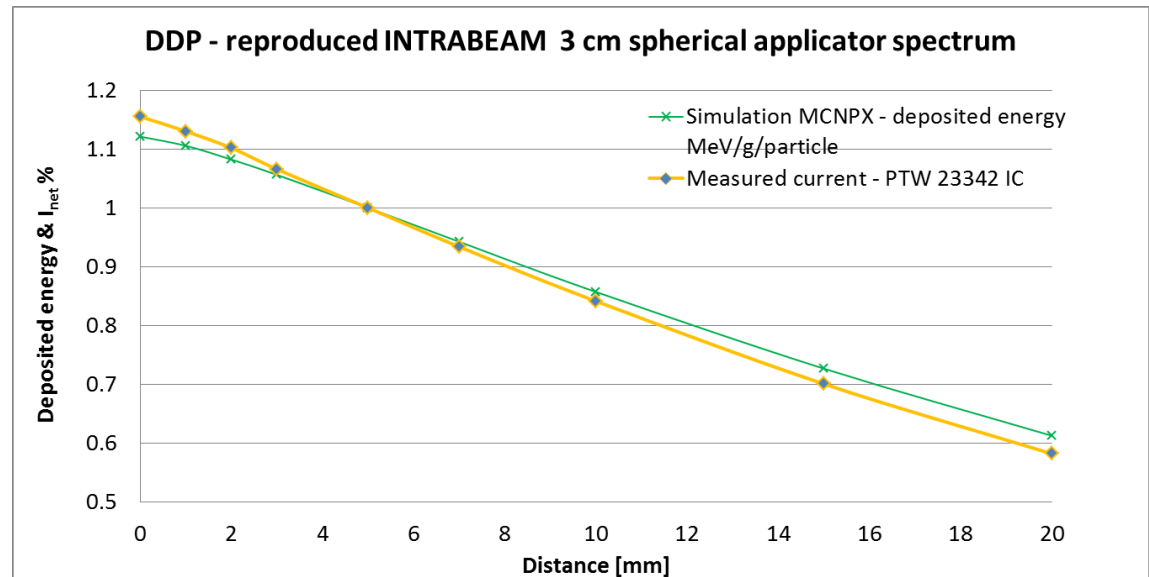
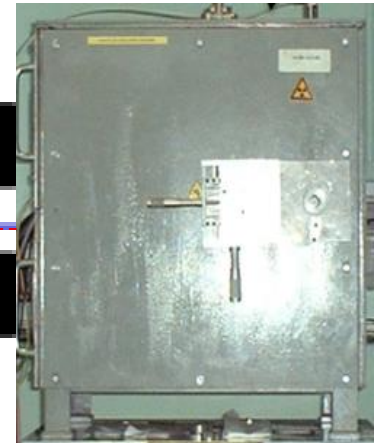
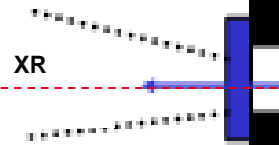
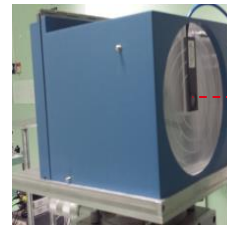
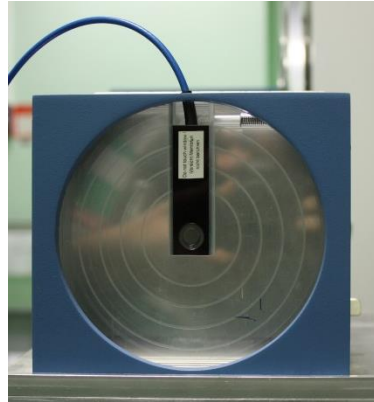
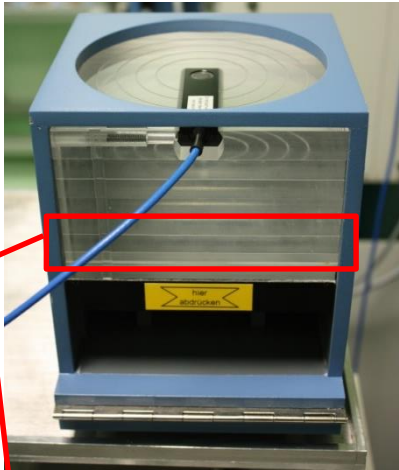
## DEPTH DOSE PROFILE DETERMINATION:

First approach to the  $D_w$



# DEPTH DOSE PROFILE DETERMINATION:

First approach to the  $D_w$

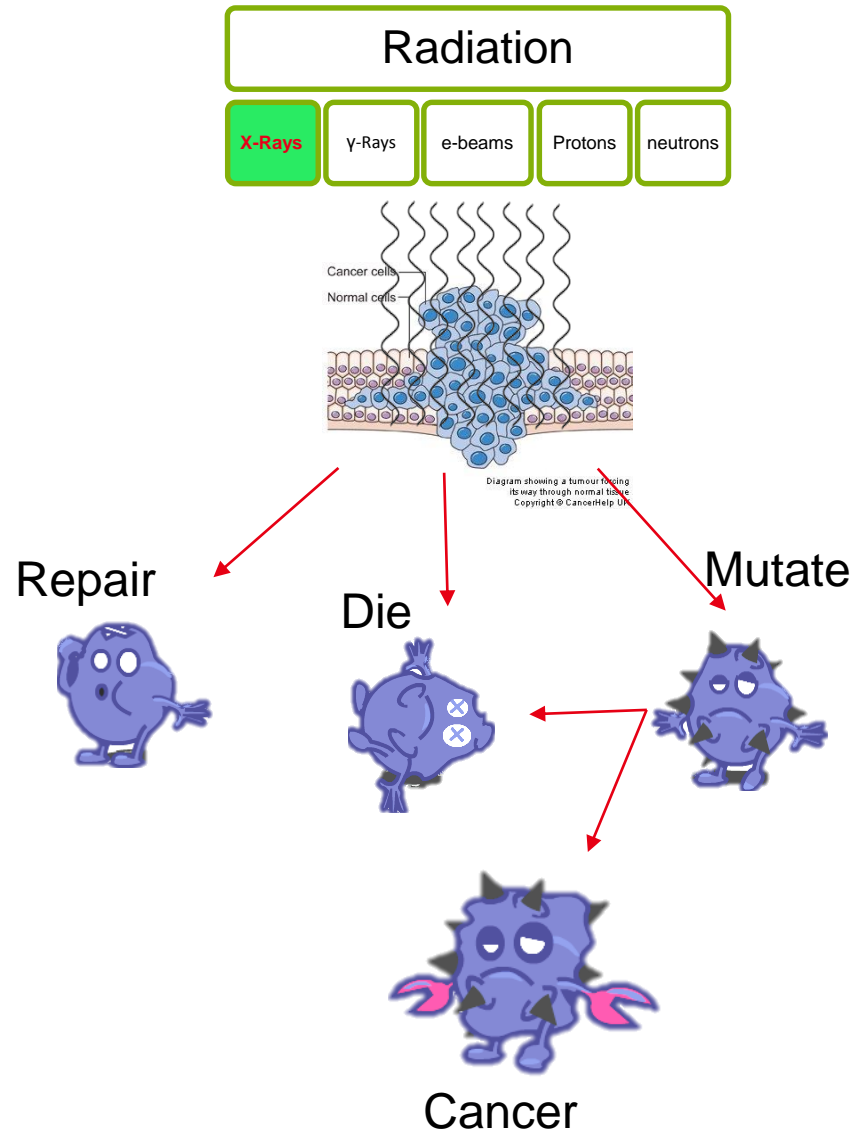


## CONCLUSIONS AND PERSPECTIVES

- Two INTRABEAM spectra were reproduced at LNHB by standard x-ray generator.
- The air kerma standard was established.
- A transfer ionization chamber was calibrated in terms of  $\dot{K}_{air}$ .
- The calibrated transfer ionization chamber was used to determine the depth dose profiles → Further analysis of the depth dose profile should be done due to an important difference between measurements and MC simulations.
- The rest of INTRABEAM applicators are to be studied in the same way.



Thank  
You





- A **calibration**, by contrast and as defined by ISO10012 is, “The set of operations which establish under specified conditions the relationship between values indicated by a measuring instrument or measuring system, or values represented by a material measure or reference material, and the corresponding value of a quantity realized by a reference standard.”
- A **reference standard**, according to ISO/BIPM/OIML, is, “A standard, generally of the highest metrological quality at a given location, from which measurements made at that location are derived.”
- A **primary standard** is operationally defined by ISO10012 as, “A standard which provides a magnitude or value of the highest accuracy (lowest) uncertainty in a given metrology discipline, for a given parameter or quantity.”
- a **measurement standard** and ISO10012 defines that as, “A material measure, measuring instrument, reference standard, material or system intended to define, realize, conserve or reproduce a unit or one or more values of quantity in order to transmit them to other measuring instruments by comparison.”

## RADIOTHERAPY

- Radiotherapy uses radiation, such as x-rays, gamma rays, electron beams or protons, to kill or damage cancer cells and stop them from growing and multiplying. It is a localized treatment, which means it generally only affects the part of the body where the radiation is directed
- Radiotherapy damages cancer cells in the region being treated. Although the radiation can also damage normal cells, they can usually repair themselves. During this repair process, you may experience some side effects, depending on the part of your body being treated.
- Depending on the type and size of the cancer, and where it is in your body, you may have one or both types of radiotherapy.
- Radiotherapy uses radiation to kill or damage cancer cells and stop them from growing and multiplying.
- Treatment also affects normal cells, but they are better able to repair themselves.
- Radiotherapy is used to treat cancer, slow its growth or relieve symptoms.
- You may have treatment in hospital or at a clinic. Most people have outpatient treatment – this means they come to each treatment session without staying in hospital.
- Radiotherapy can be given by a variety of machines and devices, depending on which part of the body is affected, and the type and stage of the tumor. The two main types are external and internal (brachytherapy or radioisotope) radiotherapy.

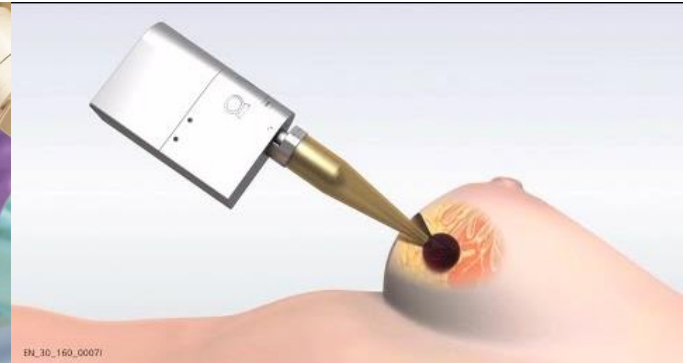
## NUCLEAR SAFETY AUTHORITY (ASN) REPORT 2012

- In France, a dozen of INTRABEAM® systems were installed since 2011.
- A call for project by the French national cancer institute (INCa) → Installation of intraoperative radiotherapy systems → breast cancer.
- One of the main objects is to reduce the treatment time

## NEED : NUCLEAR PHYSICISTS REQUEST

- The medical physicists have just the dose distributions data provided by the INTRABEAM's manufacturer.
- This data should be validated by an independent party; it calibrate the beams and determine the dose distribution.

# THE INTRABEAM SYSTEM



Skin	Vertebral column Brain
	

## DOSIMETRIC GEL

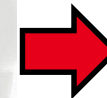
It is a system to capture the dose information in 3D.

It has many advantages:

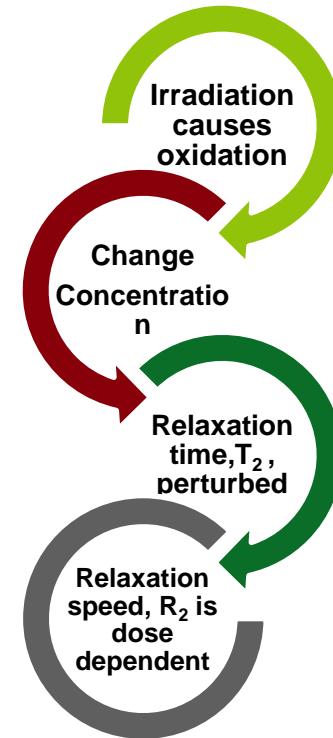
- Tissue equivalent (mostly water)
- Stabilize the dose information regarding the space and time aspects (no diffusion within the 5 hours following the irradiation).
- Could be shaped in different forms.



Reading by MRI



Determination of relative dose



## COMPARAISON MC SIMULATIONS VS. MEASUREMENTS

